

The Electroencephalogram

Basics in Recording EEG, Frequency
Domain Analysis and its Applications

Electroencephalogram (EEG)

- The EEG--an oscillating voltage recorded on scalp surface
 - Reflects Large # Neurons
 - Is small voltage
- Bands of activity and behavioral correlates
 - Gamma 30-50 Hz
 - Beta 13-30 Hz
 - Alpha 8-13 Hz
 - Theta 4-8 Hz
 - Delta 0.5-4 Hz

Delta 1-4 Hz

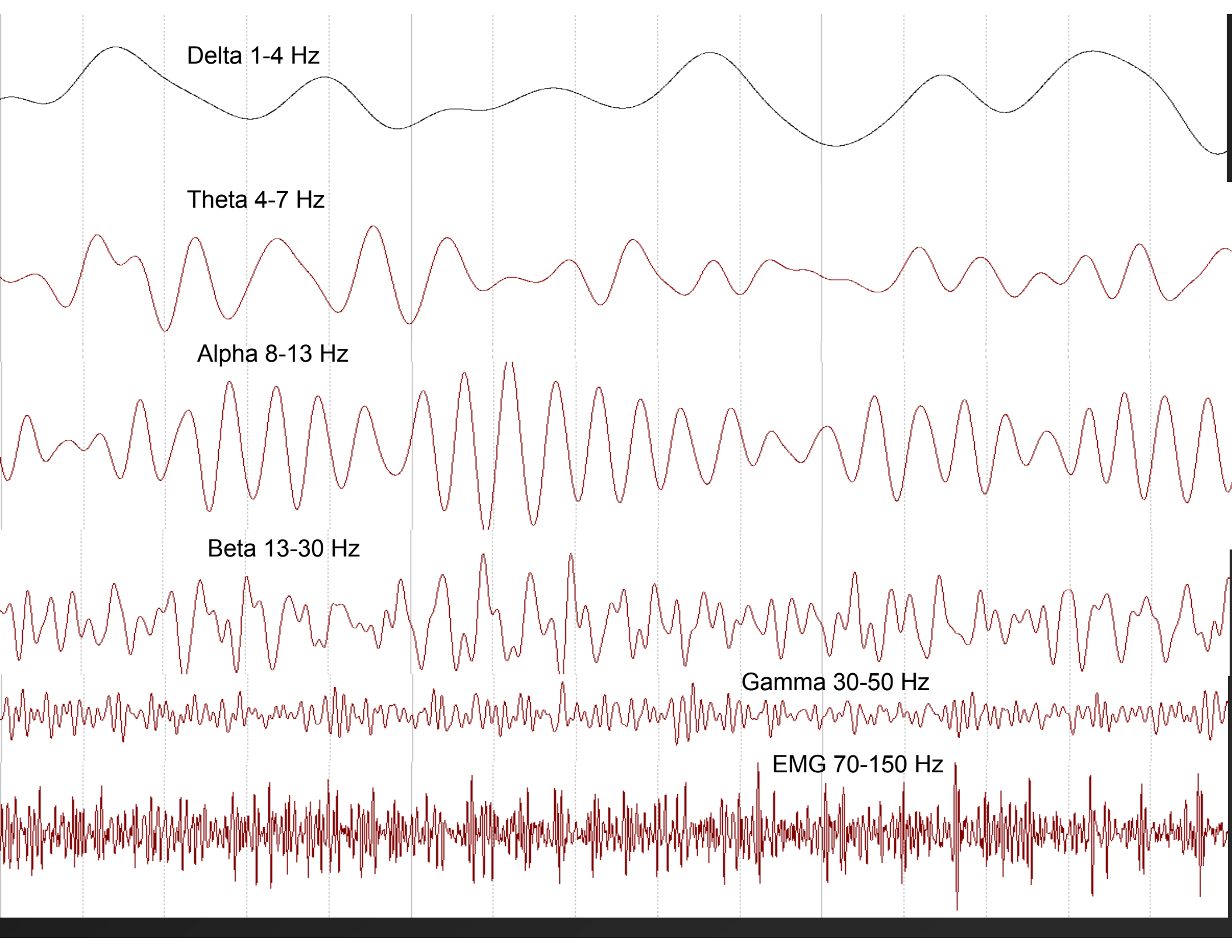
Theta 4-7 Hz

Alpha 8-13 Hz

Beta 13-30 Hz

Gamma 30-50 Hz

EMG 70-150 Hz



Utility of EEG

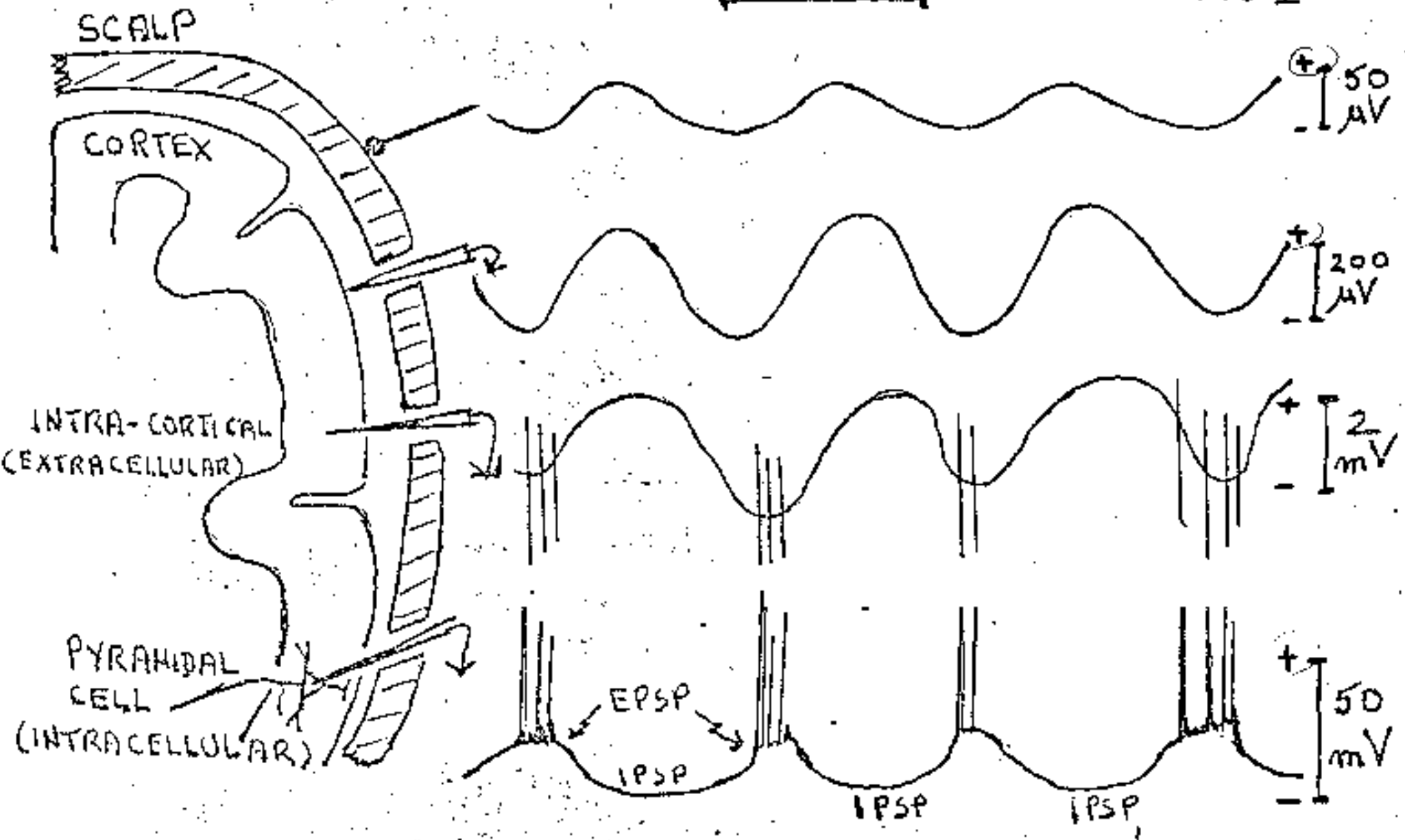
- *Relatively* noninvasive
- Excellent time resolution

Sources of scalp potentials

- Glial Cells – minimal, some DC steady potentials
- Neurons
 - Action Potentials – NO, brain tissue has strong capacitance effects, acting as Low Pass filter
 - Slow waves
 - Synaptic potentials – YES, both IPSPs and EPSPs from functional synaptic units are major contributors
 - Afterpotentials – May contribute to a lesser extent

FIG 1

0.1 SEC



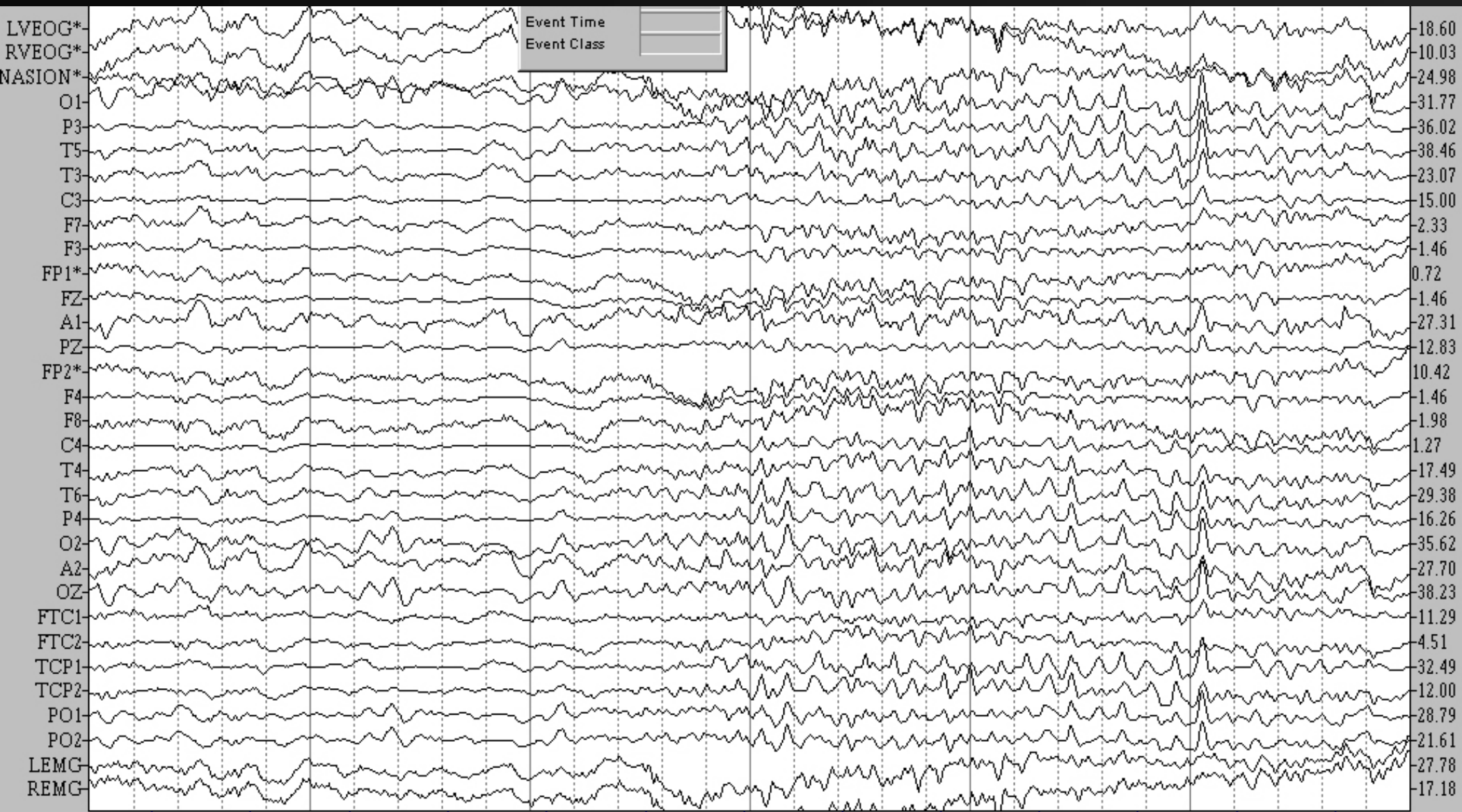
note basic similarity of wave form

Alpha and Synchronization

- Why Alpha?
 - It is obvious and hard to miss!
 - Accounts for ~70% of EEG activity in adult human brain
- From where, Alpha?
 - Historically, thought to be thalamocortical looping
 - Adrian (1935) demolished that theory
 - Recorded EEG simultaneously in cortex and thalamus
 - Damage to cortex did not disrupt thalamic alpha rhythmicity
 - Damage to thalamus DID disrupt cortical alpha rhythmicity
 - Thalamic rhythmicity remains even in decorticate preparations (Adrian, 1941)
 - Removal of ½ thalamus results in ipsilateral loss of cortical alpha

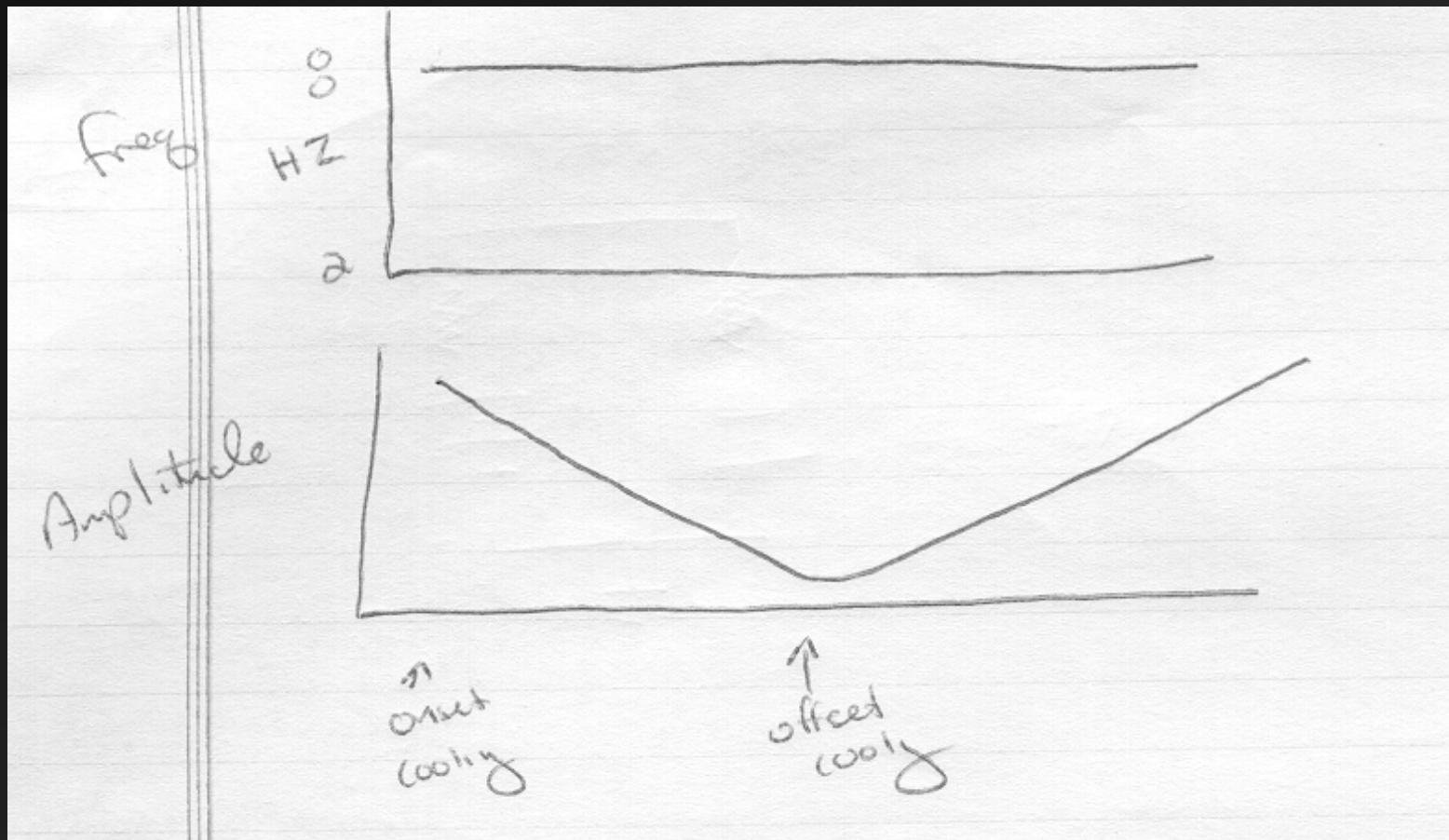
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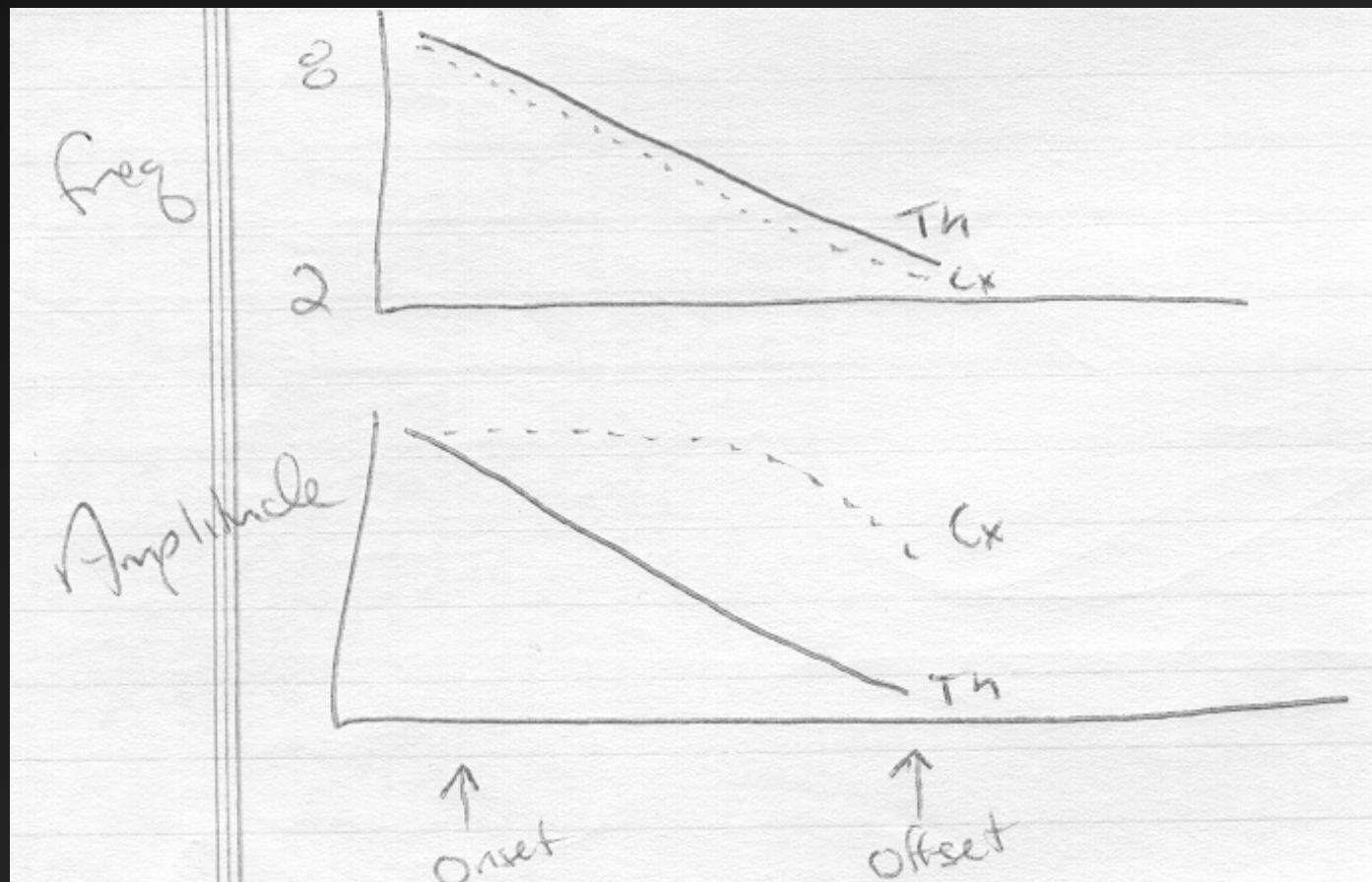
Alpha and Synchronization

- Andersen and Andersen (1968)
 - Cooling of Cortex resulted in change in amplitude but not frequency of Alpha



Alpha and Synchronization

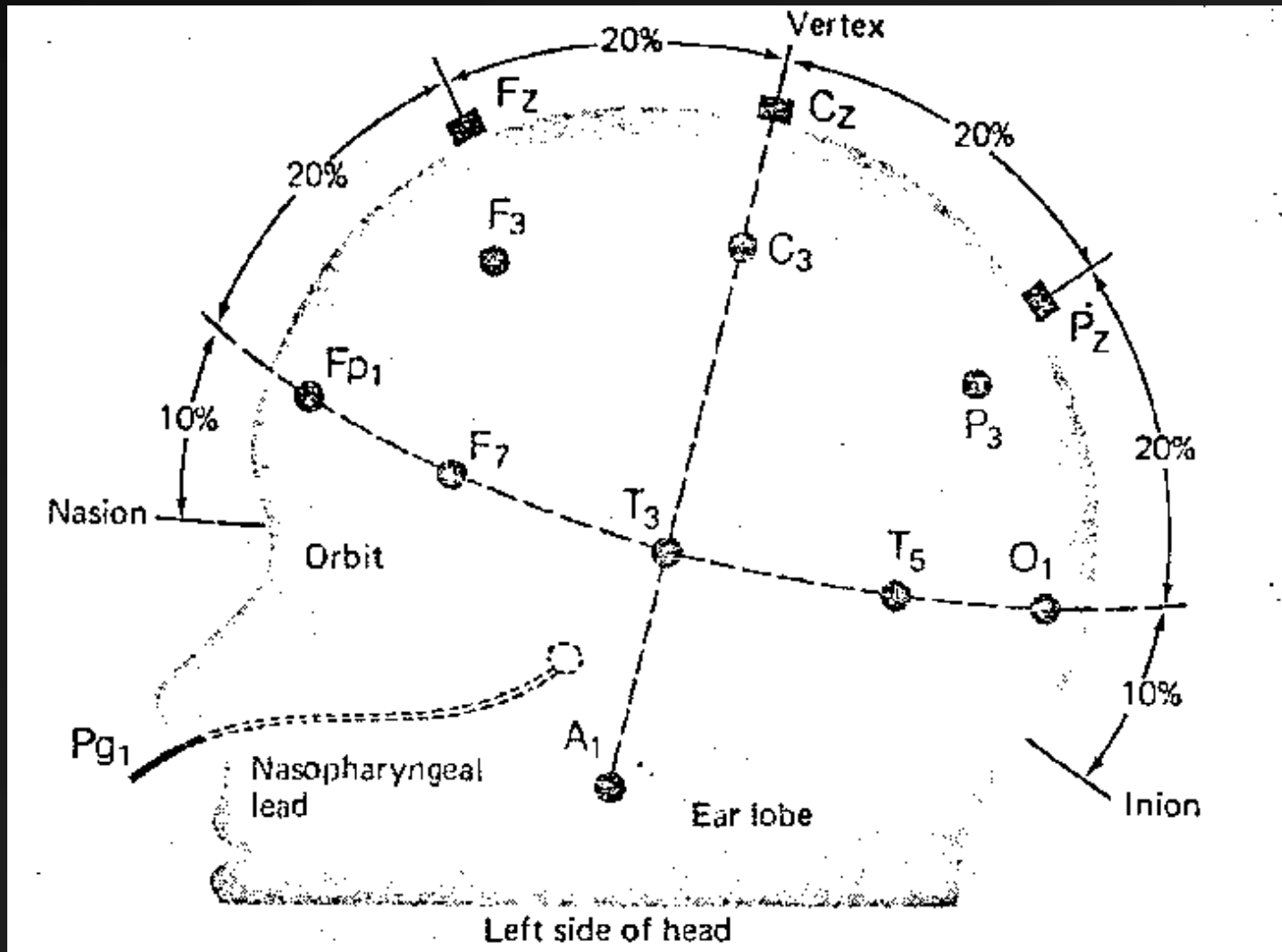
- Andersen and Andersen (1968)
 - Cooling of Thalamus resulted in change in amplitude and frequency of Alpha at both thalamus and cortex



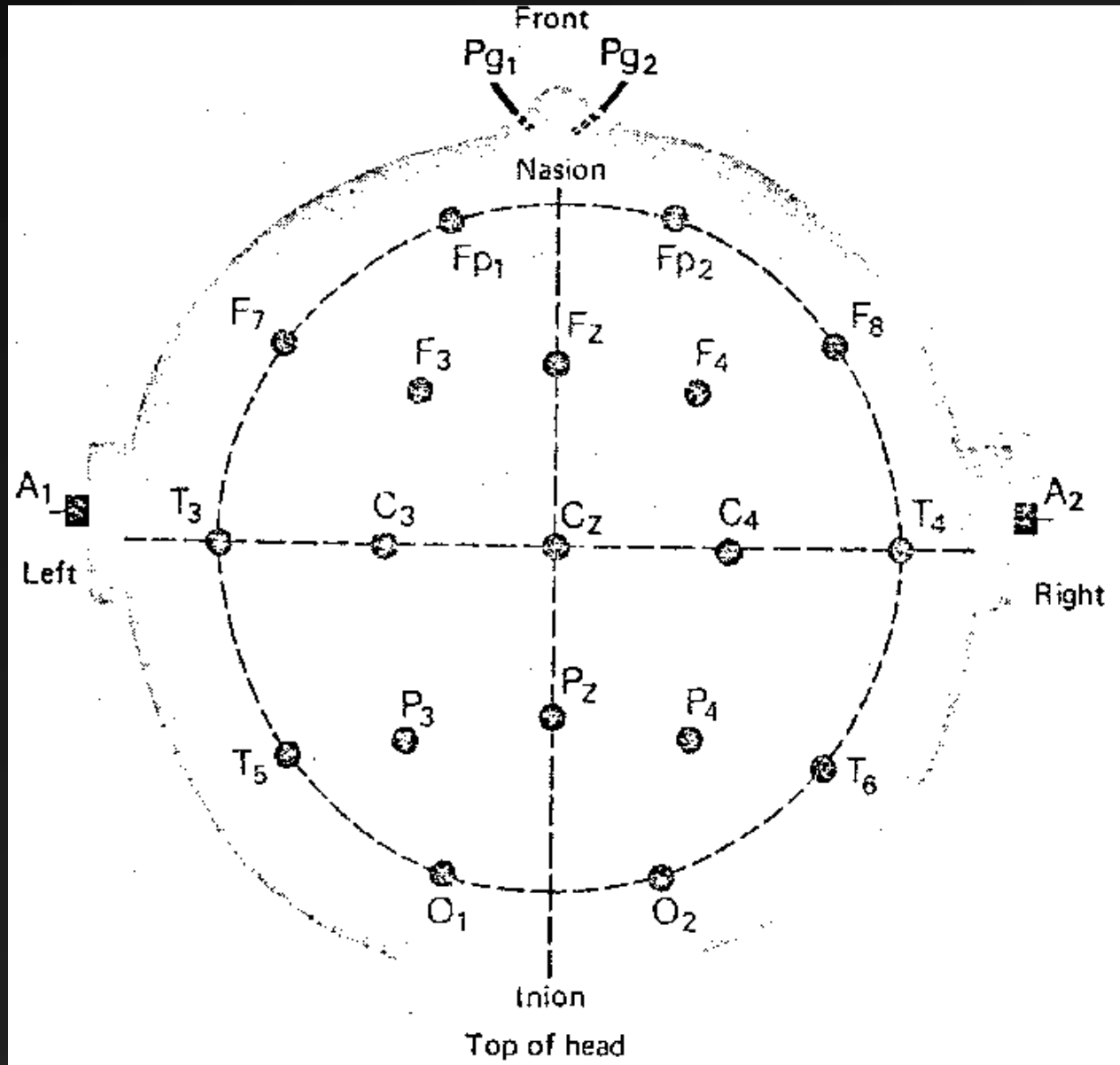
Alpha and Synchronization

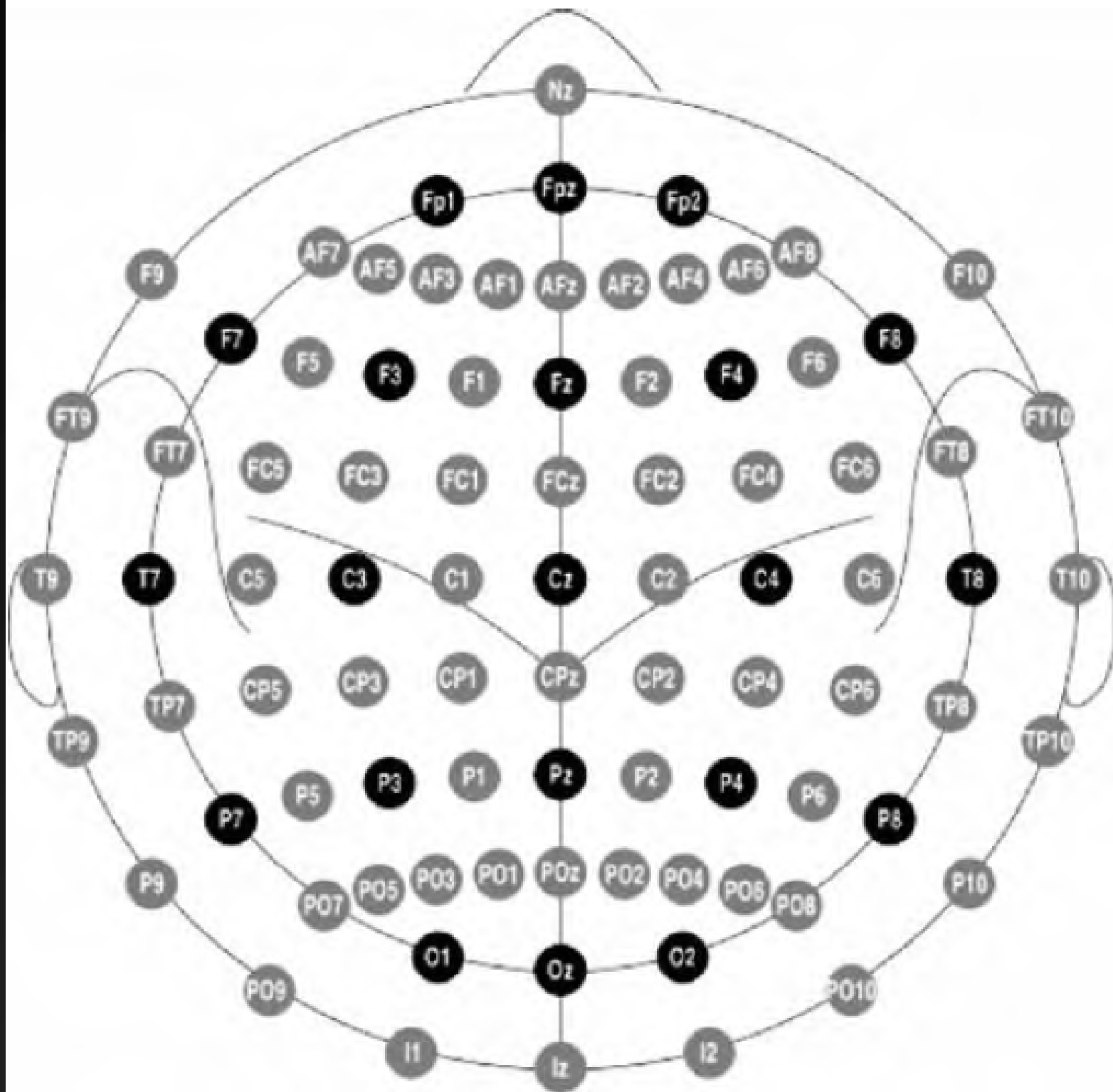
- In sum, Thalamus drives the alpha rhythmicity of the EEG
 - Cortex certainly does feedback to thalamus, but thalamus is responsible for driving the EEG
 - Particularly the Reticularis nucleus (Steriade et al. 1985)
- What causes change from rhythmicity to desynchronization?
 - Afferent input to thalamic relay nuclei
 - Mode-specific enhancement observed

Recording EEG



Recording EEG





Electrodes, Electrolyte, Preparation

- Ag-AgCl preferred, Gold OK if slowest frequencies not of interest
 - Polarizing electrodes act as capacitors in series with signal
- Electrolyte: ionic, conductive
- Affixing
 - Subcutaneous needle electrodes (OUCH)
 - Collodion (YUCK)
 - EC-2 paste; lesser of the evils
 - Electrocap

Recording References

- Measure voltage potential differences
 - Difference between what and what else?
- “Monopolar” versus Bipolar
 - No truly inactive site, so monopolar is a relative term
 - Relatively monopolar options
 - Body – BAD IDEA
 - Head
 - Linked Ears or Mastoids
 - Tip of Nose
- Reference choice nontrivial (more later) as it will change your ability to observe certain signals

Recording References

- Bipolar recording
 - Multiple active sites
 - Sensitive to differences between electrodes
 - With proper array, sensitive to local fluctuations (e.g. spike localization)
- Off-line derivations
 - Averaged Mastoids
 - Average Reference (of EEG Leads)
 - With sufficient # electrodes and surface coverage, approximates inactive site (signals cancel out)
 - Artifacts “average in”
 - Current Source Density (more in advance topics)

Dreaded Artifacts

- Three sources
 - 60-cycle noise
 - Ground subject
 - 60 Hz Notch filter
 - Muscle artifact
 - No gum!
 - Use headrest
 - Measure EMG and reject/correct for influence
 - Eye Movements
 - Eyes are dipoles
 - Reject ocular deflections including blinks
 - Use correction procedure (more in advance lecture)

AC Signal Recording Options

➤ Time Constant/HP filter

➤ Low frequency cutoff is related to TC by:

$$F = \frac{1}{(2\pi(TC))}$$

Where F = frequency in Hz, TC = Time Constant in Seconds

Applying formula:

Time Constant (sec)

Frequency (Hz)

10.00

.016

5.00

.032

1.00

.159

.30

.531

.10

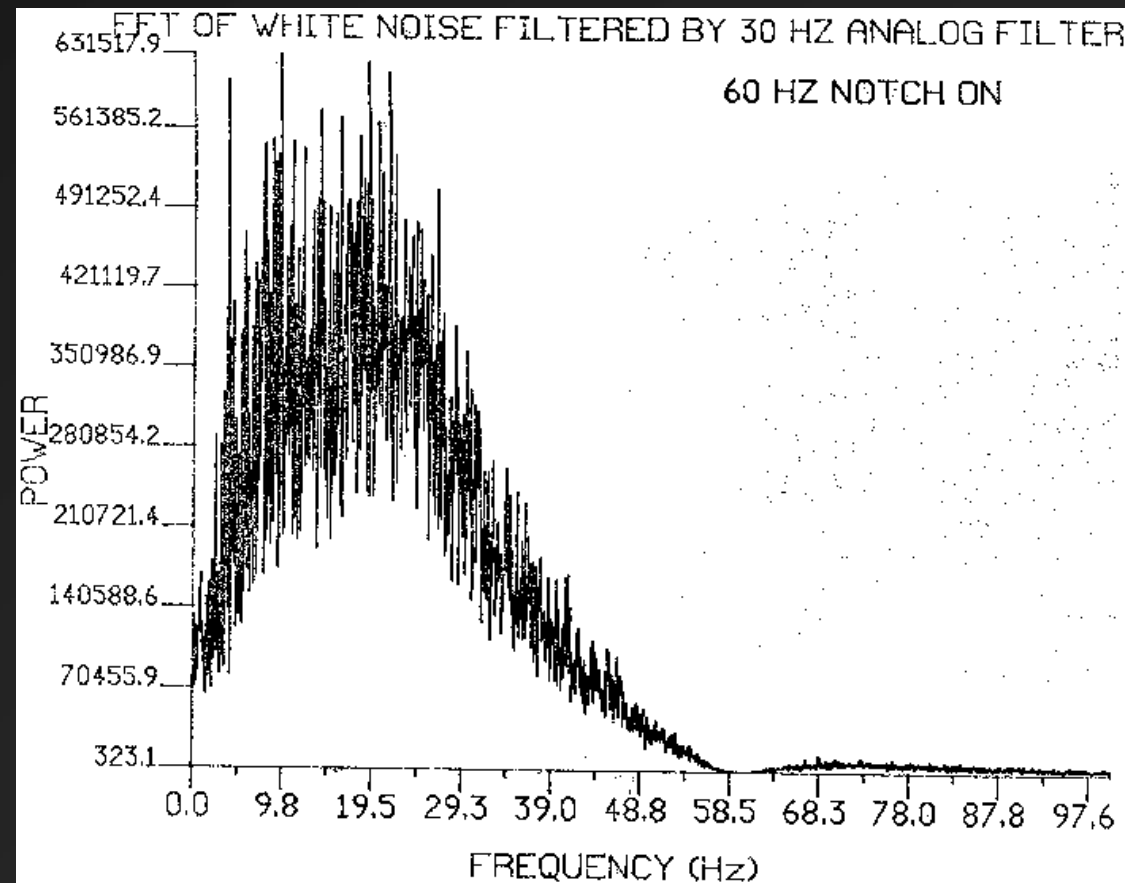
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15.915

Hi Frequency/LP Settings

- Do not eliminate frequencies of interest
- Polygraphs have broad roll-off characteristics
- Be mindful of digitization rate (more info soon!)



Digital Signal Acquisition

- Analog Vs Digital Signals
 - Analog
 - Continuously varying voltage as fxn of time
 - Discrete Time
 - Discrete points on time axis, but full range in amplitude
 - Digital
 - Discrete time points on x axis represented as a limited range of values (usually 2^x , e.g $2^{12} = 4096$)

A/D converters

- Schmidt Trigger as simple example
- The A/D converter (Schematic diagram)
 - Multiplexing (several channels); A/D converter is serial processor
 - Result is a vector [1 x n samples] of digital values for each channel ($[x(t_0), x(t_1), x(t_2), \dots, x(t_{n-1})]$)
 - 12 bit converters allow $2^{12} = 4096$ values
 - 16 bit converters allow $2^{16} = 65536$ values
- 12 bit is adequate for EEG
 - 4096 values allow 1 value for each ~ 0.02 μ volts of scalp voltage (depending upon sensitivity of amplifier, which will amplify signal $\sim 20,000$ times before polygraph output)
 - e.g.,
 - $2.1130 \mu\text{volts} \Rightarrow 2481 \text{ D.U.'s (2480.74)}$
 - $2.1131 \mu \text{ volts} \Rightarrow 2481 \text{ D.U.'s (2480.76)}$
 - $2.1250 \mu \text{ volts} \Rightarrow 2483 \text{ D.U.'s (2483.20)}$

SOUND RECORDING

There are two basic methods of recording voices and music — analog and digital. In analog recording, the recording medium varies continuously in a way that is similar to or analogous to the incoming signal. In digital recording, the signal is sampled electronically and recorded as a rapid sequence of separate coded measurements. Both analog and digital

recording preserve the varying voltage of the sound signal produced by a microphone, but of the two, digital recording is the more accurate. In addition, a certain amount of electrical noise or hiss always enters the recording process. Digital recording is insensitive to this noise, whereas analog recording requires noise reduction systems.

SOUND SIGNAL

The curve represents the varying voltage of the electrical sound signal produced when a sound wave strikes a microphone. The varying levels of the voltage are produced by the varying pressures of the sound wave, so the curve also represents the changing energy of the sound wave. The voltage varies within a limited range, from silence to maximum volume.



STEREO

In stereophonic sound, two separate tracks or channels of sound are recorded — one to the left and one to the right. When the two channels are reproduced through loudspeakers the sounds seem to have locations in space.



VOLTAGE

LEVEL

7

6

5

4

3

2

1

0

ORIGINAL SIGNAL WAVEFORM

ANALOG TAPE

An analog tape records the sound signal as a continuous wave of magnetism. The magnetism may have any value within a limited range, varying by the same amount as the sound signal voltage.

VOLTAGE

SAMPLES

ANALOG RECORDING

In an analog recording, the varying voltage of the electric signal from the microphone is changed into another quantity that varies by the same amount. In a tape recording, the signal goes to a record head that magnetizes the particles in a moving tape. In an analog tape, the degree of magnetization on the tape corresponds to the amount of voltage in the signal.

DIGITAL TAPE

The sound signal is saved as a precise sequence of areas of high and low magnetism. These represent the ones and zeros of the binary code.

COMPACT DISK

In this digital system, areas of low binary code have pits in the surface of the disk. One represents the ones and zeros of the binary code.

DIGITAL RECORDING

A digital recording consists of rapid measurements of the sound wave in the form of on-off binary codes (here represented by ones and zeros). The electric signal from the microphone is sampled more than 40,000 times a second. The number of bits in each sample is converted into a binary code (see p.332) consisting of on-off electric pulses. Here 3-bit (three digit) codes are shown for simplicity, so that 5 volts becomes 101 (on-off-on). In practice, 16-bit codes are used to distinguish more than 65,000 levels of voltage and so produce extremely accurate samples. The resulting on-off signals are then recorded on digital tape as high-low sequences of magnetism. In a compact disk (see pp.248-9), these codes become sequences of minute pits produced by a laser beam.

The Problem of Aliasing

➤ Definition

- To properly represent a signal, you must sample at a fast enough rate.
- Nyquist's (1928) theorem
 - a sample rate twice as fast as the highest signal frequency will capture that signal perfectly
 - Stated differently, the highest frequency which can be accurately represented is one-half of the sampling rate
 - This frequency has come to be known as the Nyquist frequency and equals $\frac{1}{2}$ the sampling rate

➤ Comments

- Wave itself looks distorted, but frequency is captured adequately.
- Frequencies faster than the Nyquist frequency will not be adequately represented
- Minimum sampling rate required for a given frequency signal is known as Nyquist sampling rate



Harry Nyquist

Aliasing and the Nyquist Frequency

- In fact, frequencies above Nyquist frequency represented as frequencies lower than Nyquist frequency
 - $F_{Ny} + x \text{ Hz}$ will be seen as $F_{Ny} - x \text{ Hz}$
 - “folding back”
 - frequency $2F_{Ny}$ seen as 0,
 - frequency $3F_{Ny}$ will be seen as F_{Ny}
 - accordion-like folding of frequency axis

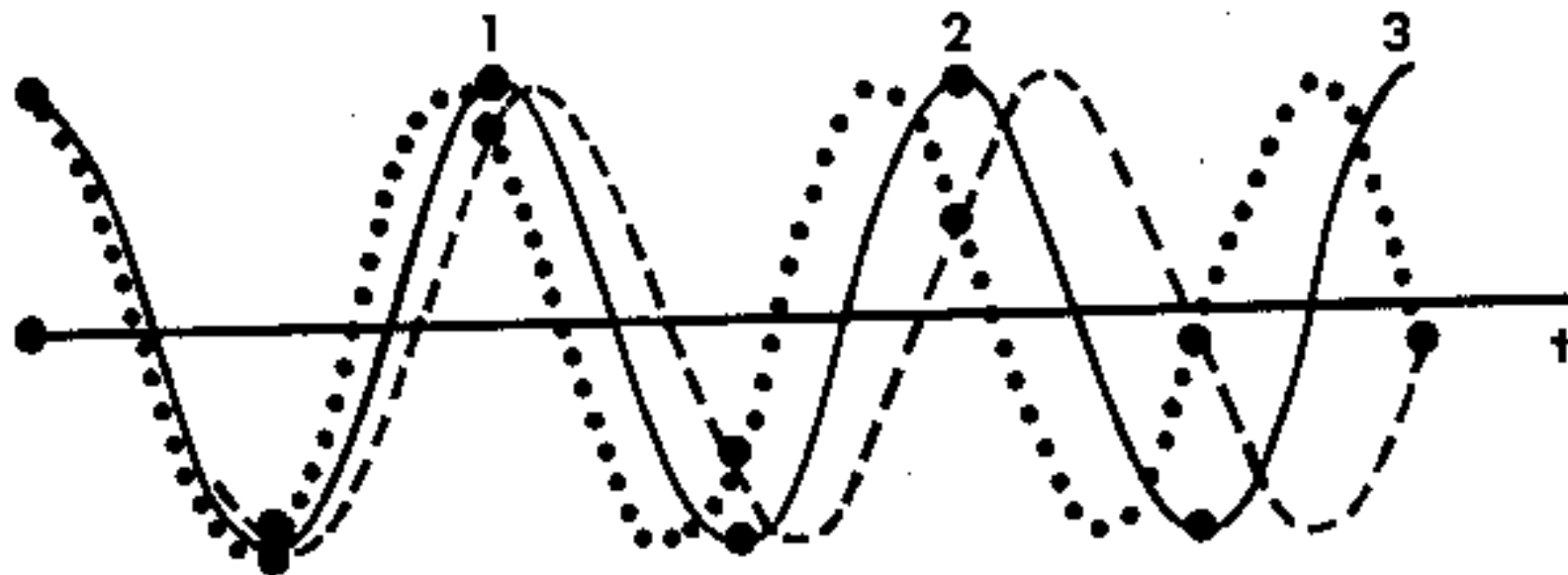


Fig. 3.1. A cosine wave of frequency F (solid line) sampled at its Nyquist rate. A higher frequency (dotted) wave, frequency $F + a$, is shown sampled at the same rate. At the sample times it is indistinguishable from a lower frequency (dashed) wave, frequency $F - a$.

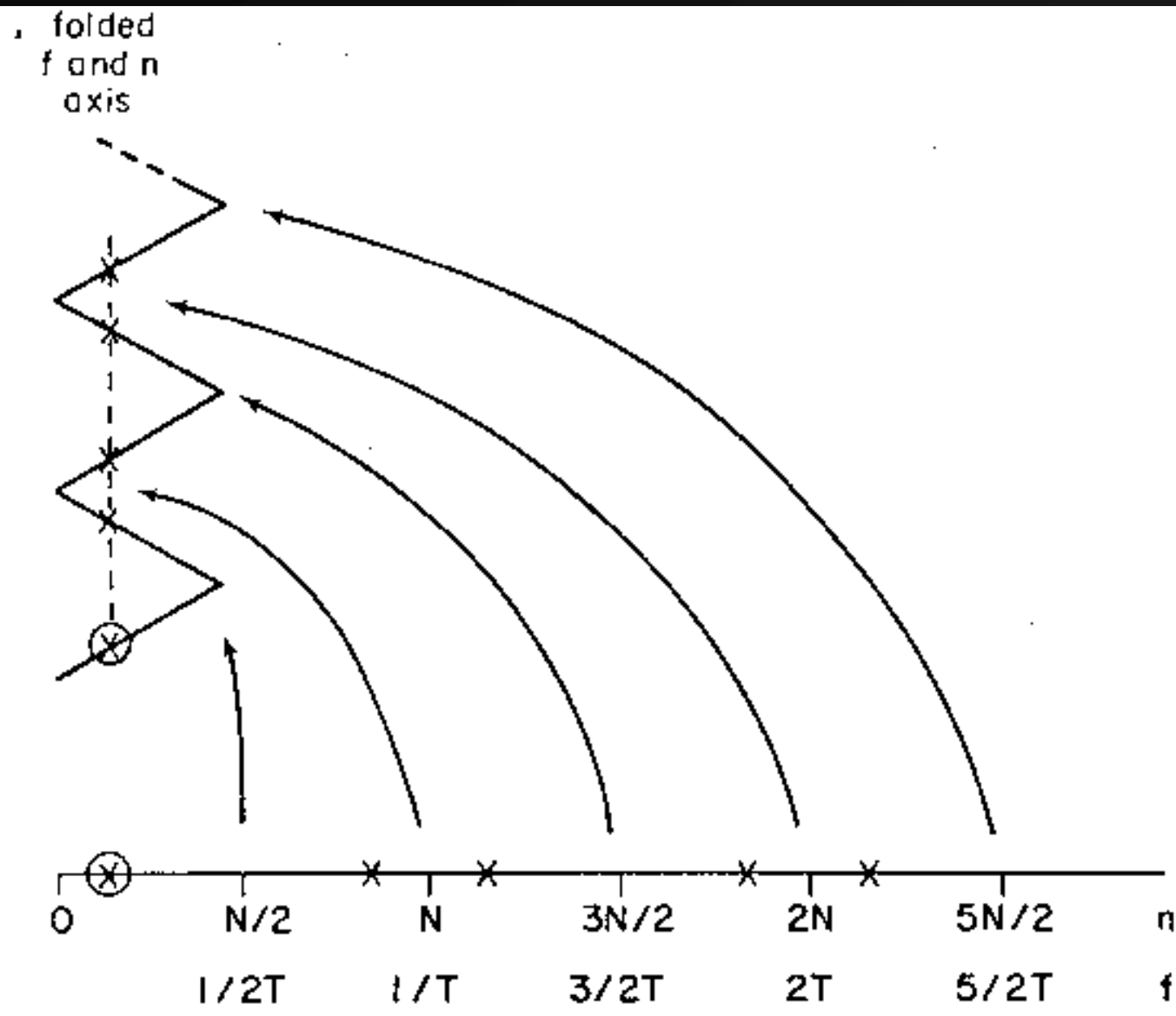
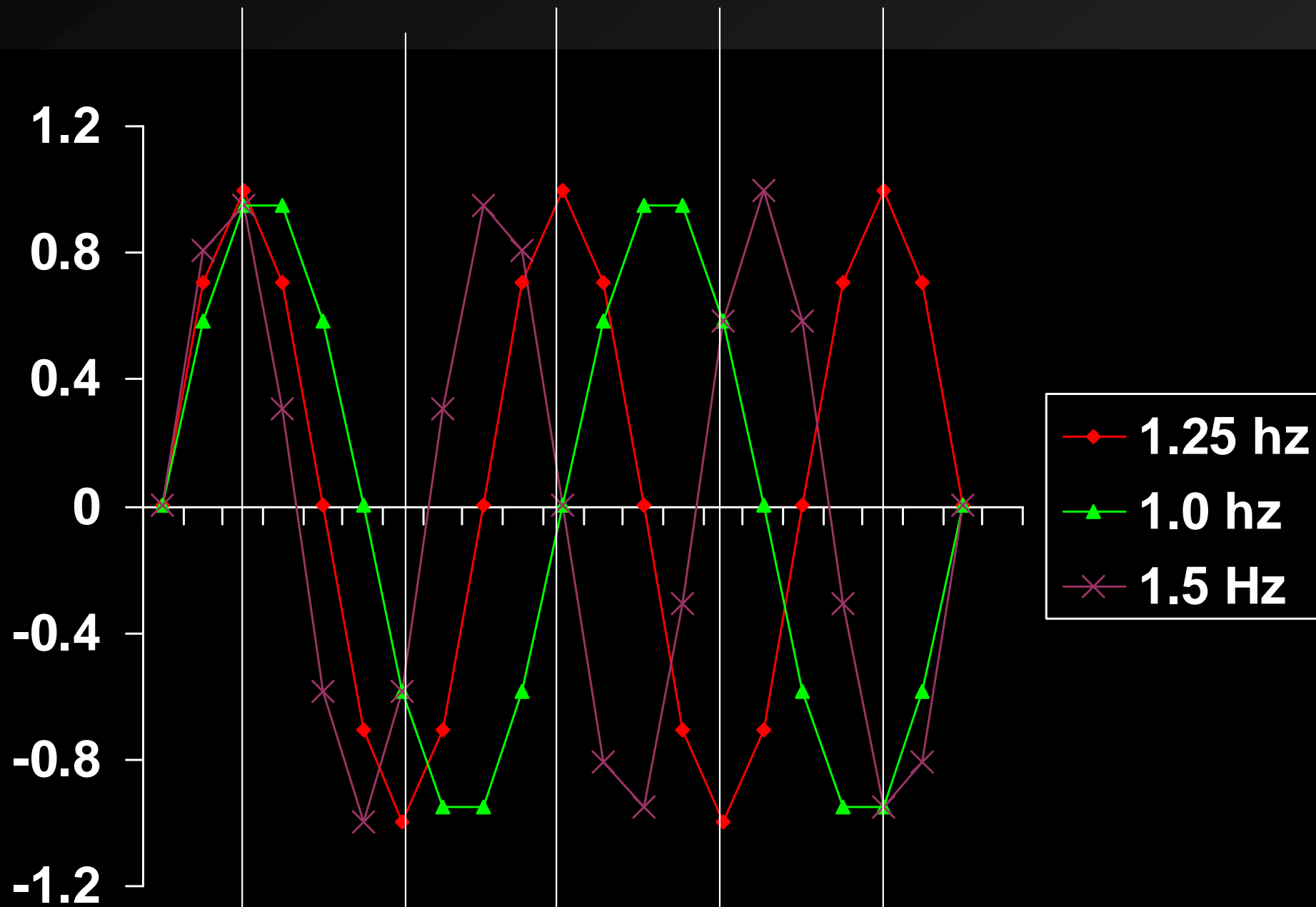
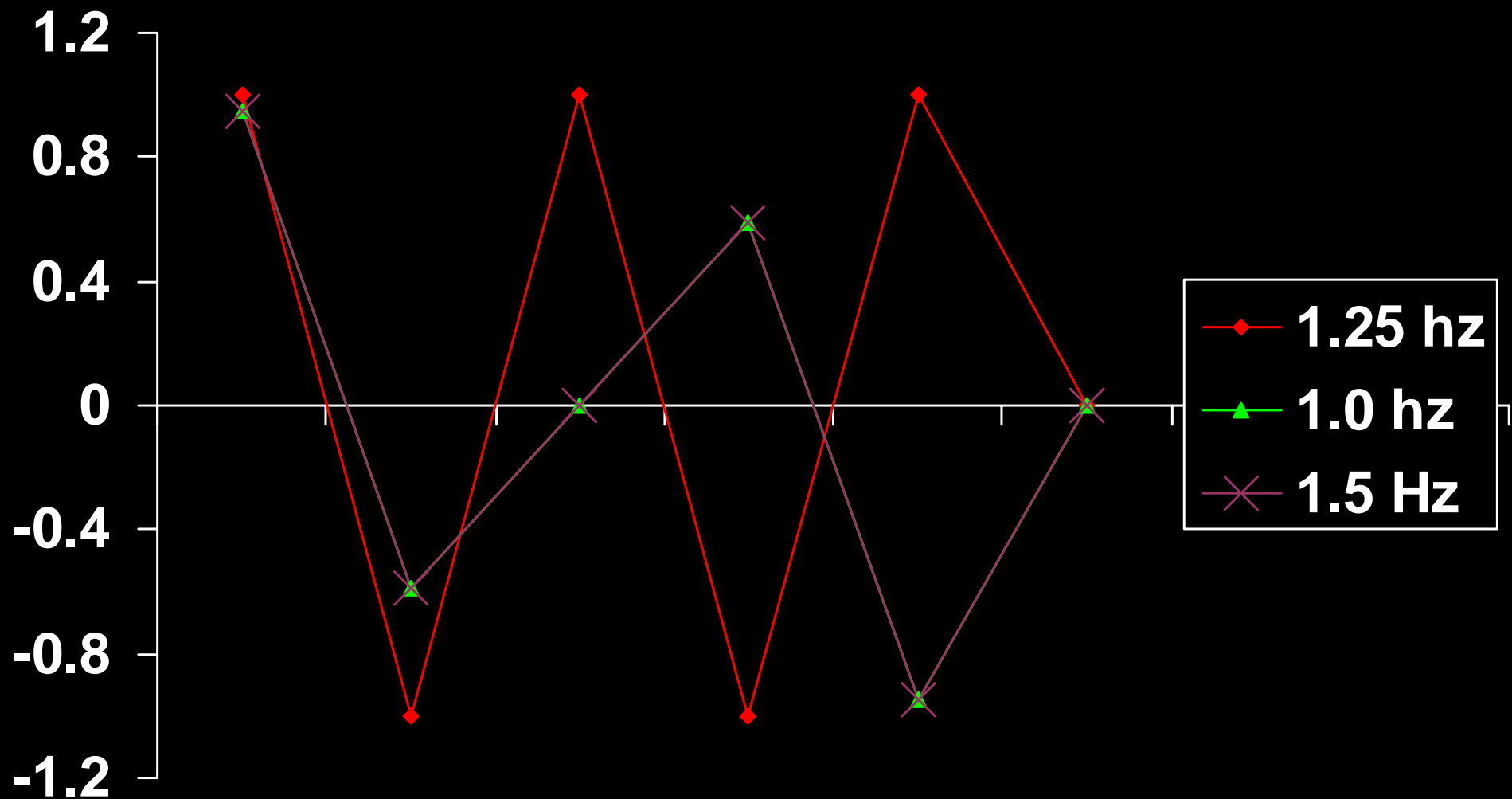


Fig. 3.2. The accordionlike folding of the frequency (or n) axis due to sampling of a continuous signal. Frequency components of the original signal marked with x 's on the f axis are interpreted in the sampled version as belonging to the lowest frequency, an encircled x .

Aliasing Demo (Part 1, 10 Hz Sampling Rate)



Aliasing Demo (Part 2, 2.5 Hz Sampling Rate)



Solutions to Aliasing

- Sample very fast
- Use anti-aliasing filters
- **KNOW YOUR SIGNAL!**

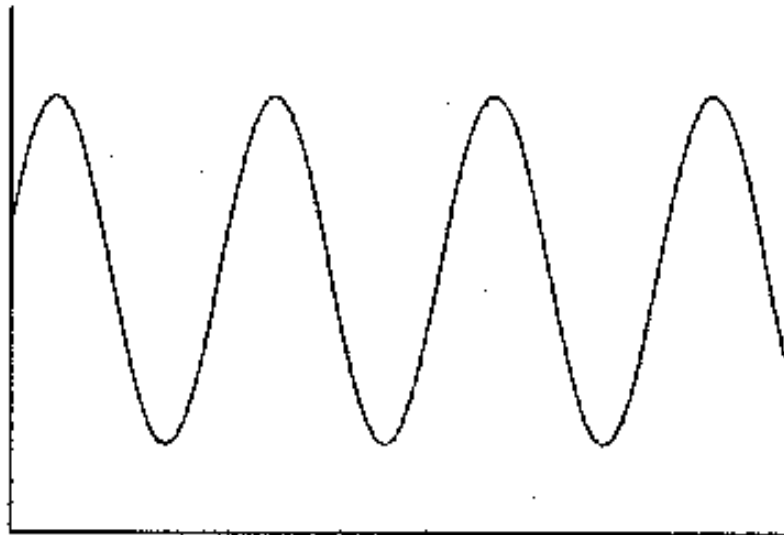
Time Domain Vs Frequency Domain Analysis

- Time Domain Analysis involves viewing the signal as a series of voltages as a function of time, $[x(0), x(t_1), x(t_2), \dots, x(t_{n-1})]$
 - e.g., skin conductance response, event-related potential
 - Relevant dependent variables
 - latency of a particular response
 - amplitude of that response within the time window
- More about time domain next time

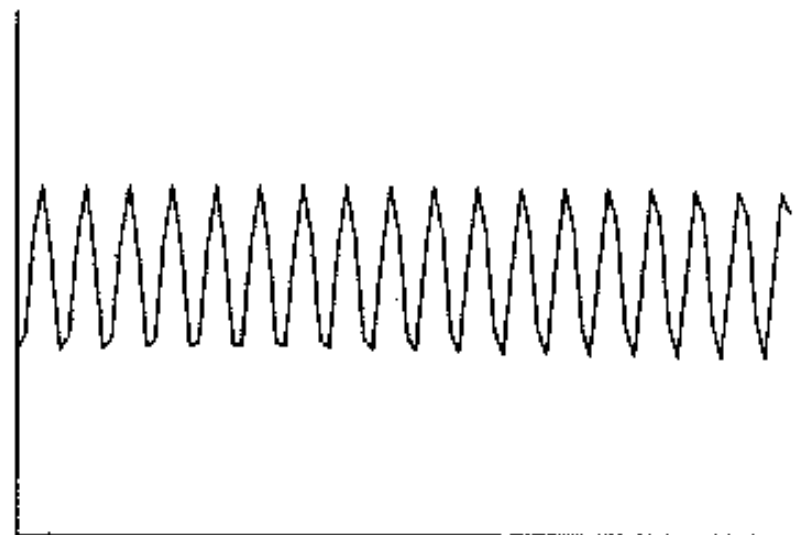
Time Domain Vs Frequency Domain Analysis

- Frequency Domain Analysis involves characterizing the signal in terms of its component frequencies
 - Assumes periodic signals
- Periodic signals (definition):
 - Repetitive
 - Repetitive
 - Repetition occurs at uniformly spaced intervals of time
- Periodic signal is assumed to persist from infinite past to infinite future

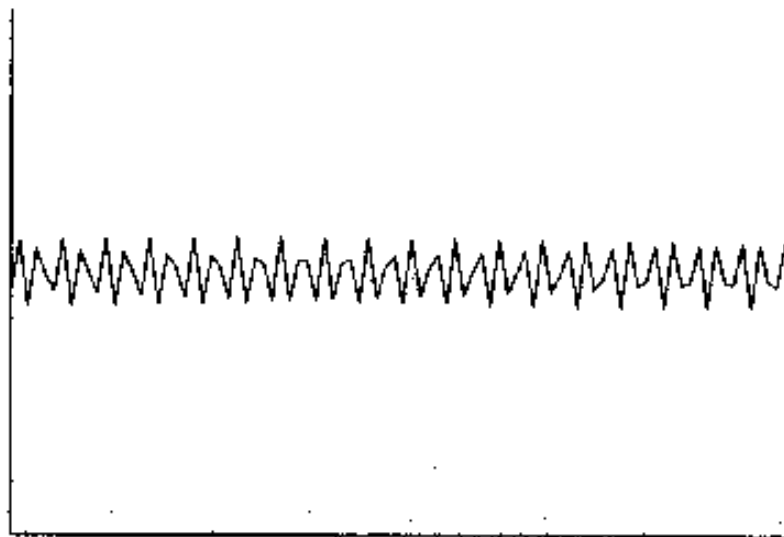
Wave 1



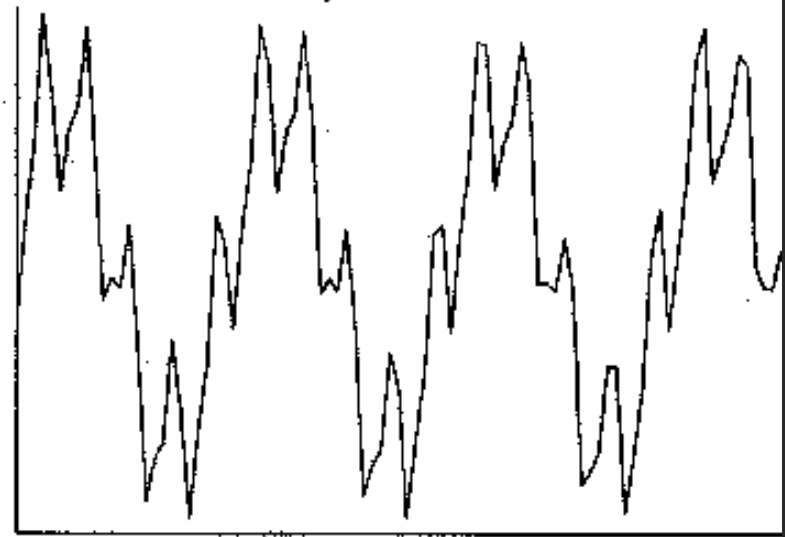
Wave 2



Wave 3



Composite Wave



Fourier Series Representation

- If a signal is periodic, the signal can be expressed as the sum of sine and cosine waves of different amplitudes and frequencies
- This is known as the Fourier Series Representation of a signal
- In Conceptual (but mathematically imprecise) terms:

$$x(t) = \text{Phase}(t_0) + \sum_1^N \frac{1}{2} [\text{Amp}_{\cos} * \cos(\text{fxn}(n, t, T)) + \text{Amp}_{\sin} * \sin(\text{fxn}(n, t, T))]$$

Where

Where N=number of samples

T=period sampled by the N samples

n=frequency from 0 to Nyquist, in 1/T increments

Fourier Series Representation

➤ Pragmatic Details

- Lowest Fundamental Frequency is $1/T$
- Resolution is $1/T$

➤ Phase and Power

- There exist a phase component and an amplitude component to the Fourier series representation
 - Using both, it is possible to completely reconstruct the waveform.

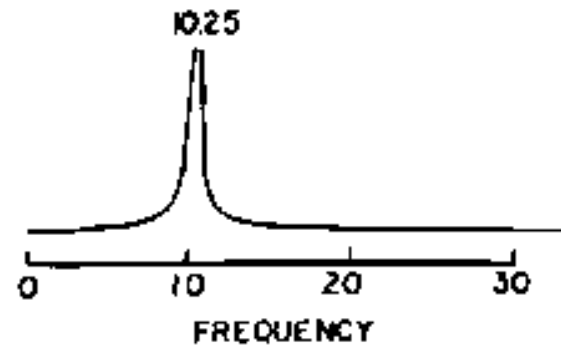
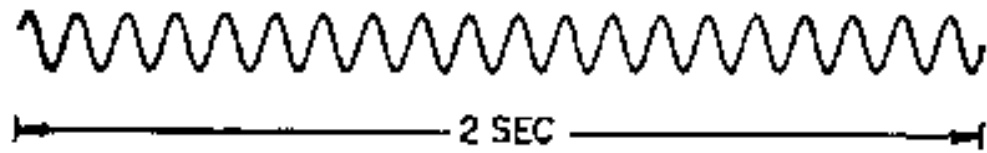
➤ Psychophysicist often interested in amplitude component:

- Power spectrum; for each frequency n/T

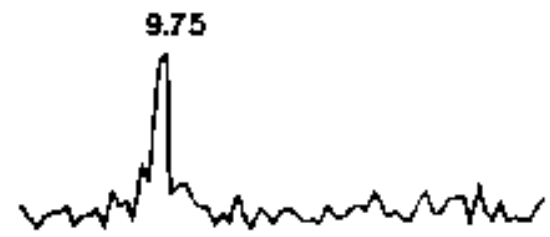
$$|\text{Amp}_{\cos}^2 + \text{Amp}_{\sin}^2|$$

- Amplitude Spectrum (may conform better to assumptions of statistical procedures); for each frequency n/T

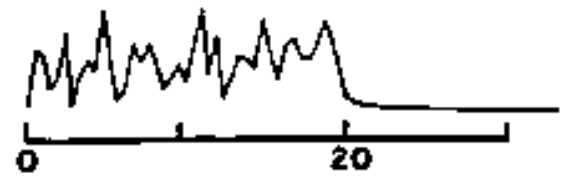
$$|\text{Amp}_{\cos}^2 + \text{Amp}_{\sin}^2|^{1/2}$$



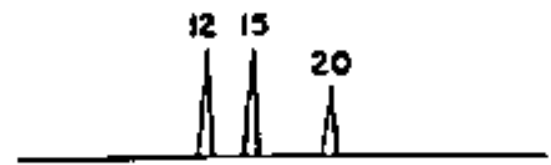
d



b



c



d

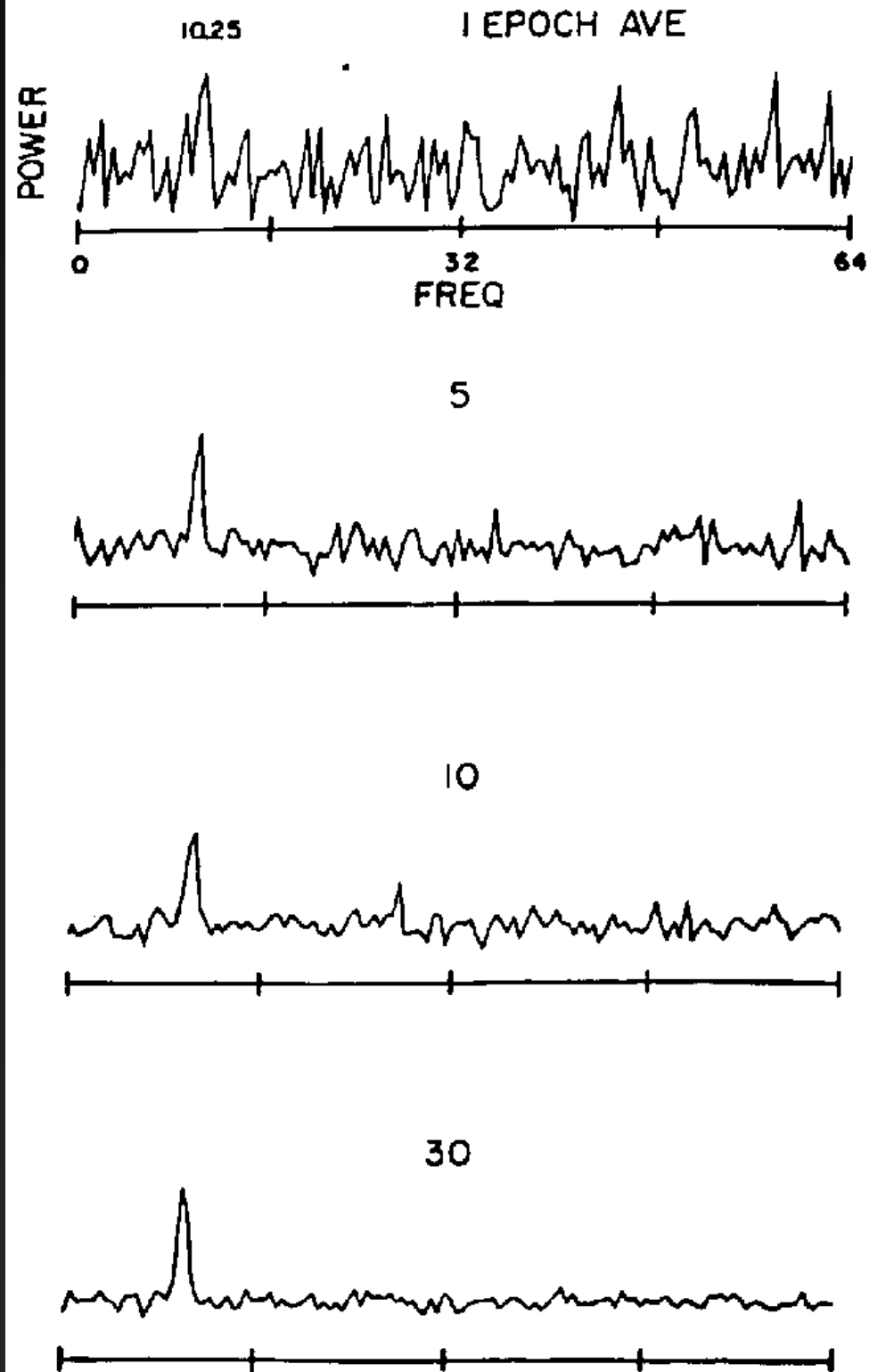
Time Domain

Frequency Domain

...

Averaging Multiple Epochs improves ability to resolve signal

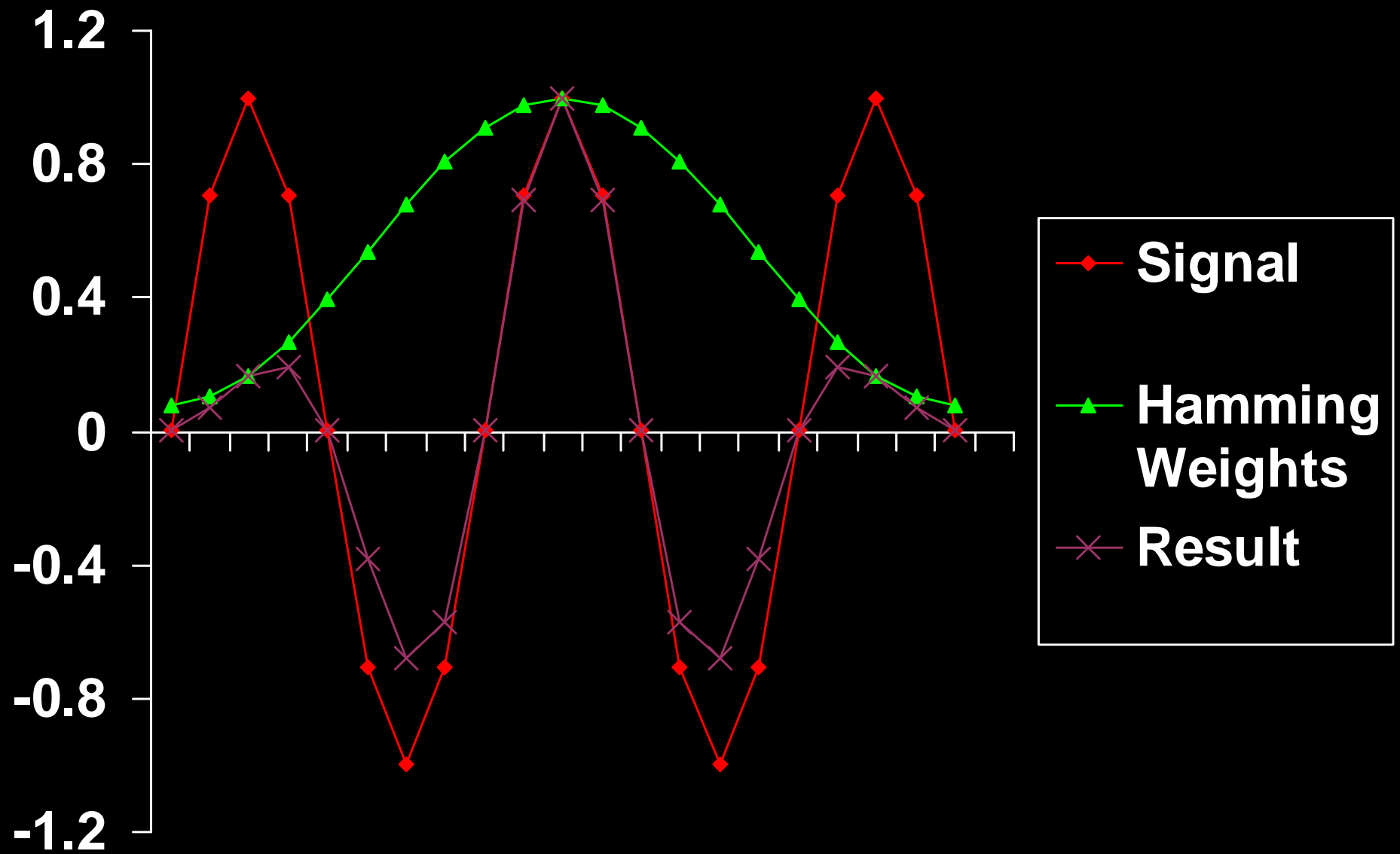
Note noise is twice
amplitude of the signal



Lingering details

- In absence of phase information, it is impossible to reconstruct the original signal
 - **Infinite** number of signals that could produce the same amplitude or power spectrum
- Spectra most often derived via a **Fast Fourier transform (FFT)**; a fourier transform of a discretely sampled band-limited signal with a power of 2 samples
- Sometimes **autocovariance function** is used (a signal covaries with itself at various phase lags; greater covariation at fundamental frequencies)
- Windowing: the Hamming Taper

Hamming Demo



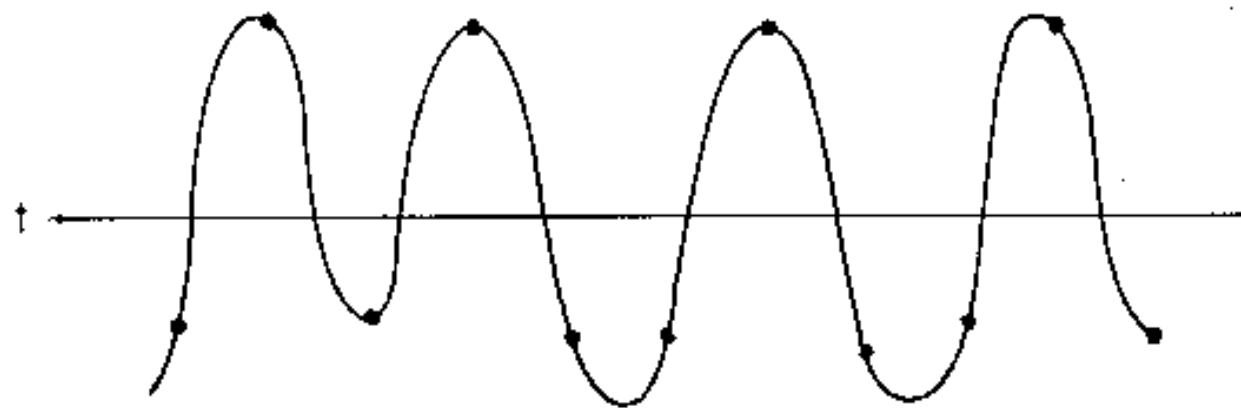
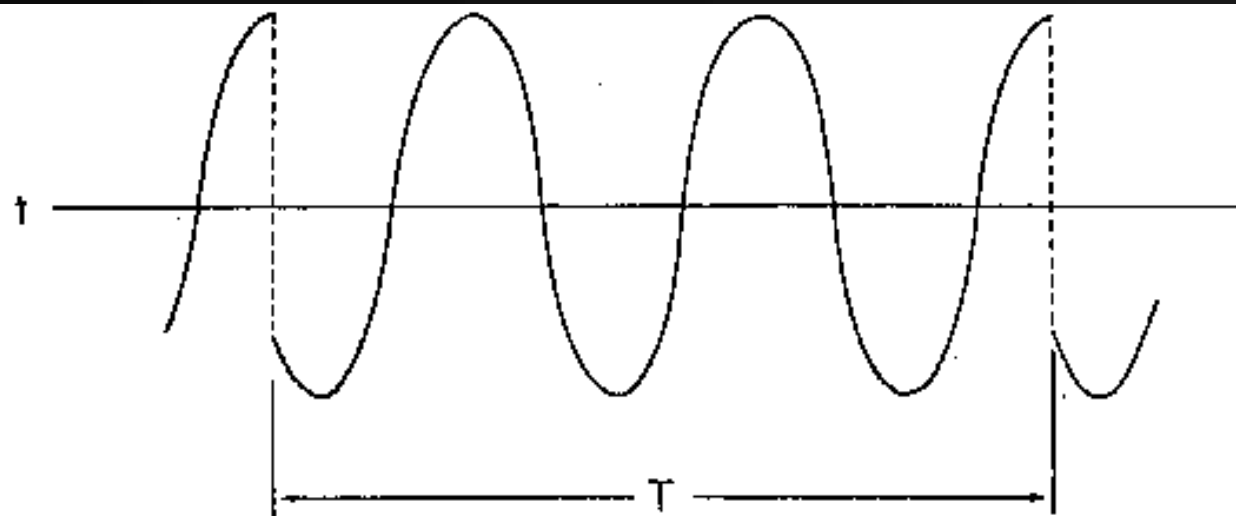
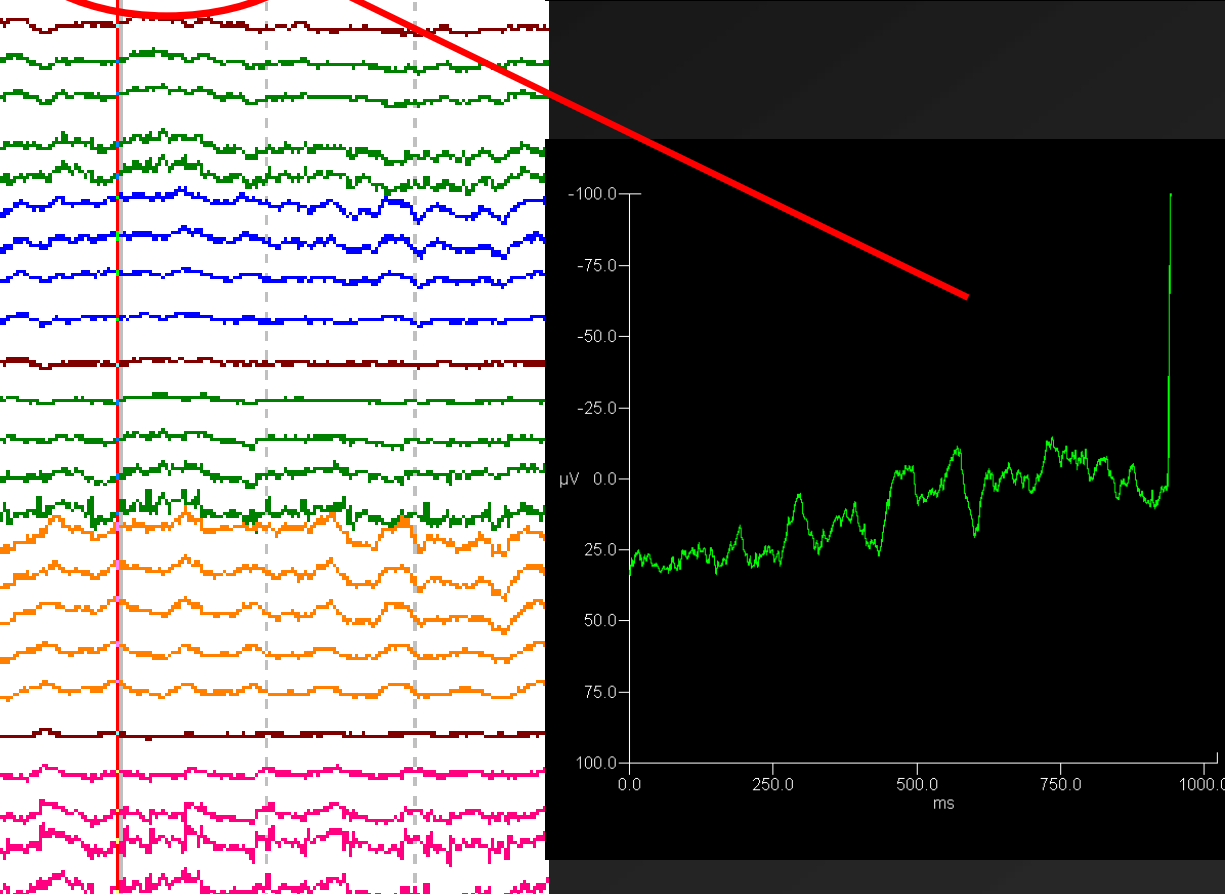
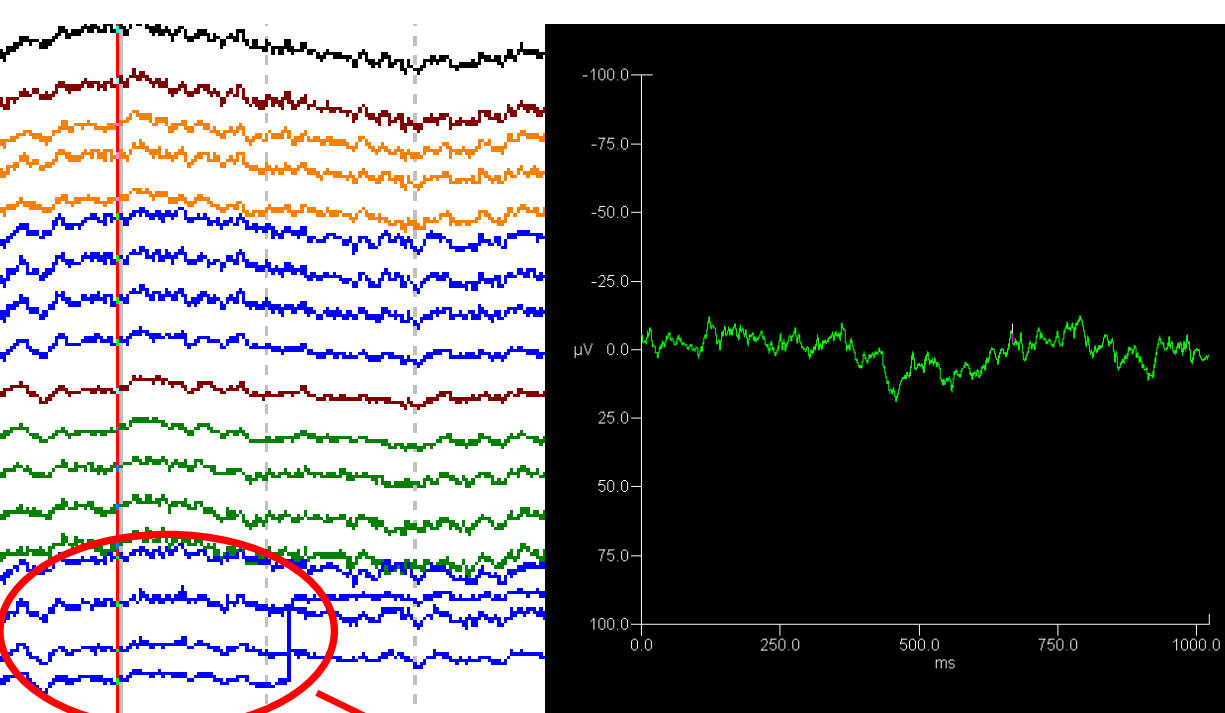


Fig. 3.3. Top, a periodicized segment of a cosine wave. T is the observation time and $3T/8$ the period of the wave. Note the discontinuities at 0 and T . Bottom, a continuous and periodic band-limited wave drawn through the sample points $\Delta = T/16$ sec apart.

Pragmatic Concerns

- Sample fast enough so no frequencies exceed Nyquist
 - signal bandwidth must be limited to less than Nyquist
 - Violation = **ERROR**
- Sample a long enough epoch so that lowest frequency will go through at least one period
 - Violation = **ERROR**
- Sample a periodic signal
 - if subject engaging in task, make sure that subject is engaged during entire epoch
 - Violation = ??, probably introduce some additional frequencies to account for change



Applications

➤ Emotion Asymmetries

➤ Lesion findings

➤ Catastrophic reaction (LH)

➤ RH damage show a belle indifference

➤ EEG studies

➤ Trait (50+ studies)

➤ State (30 + studies)



Most of them positive!

Types of Studies

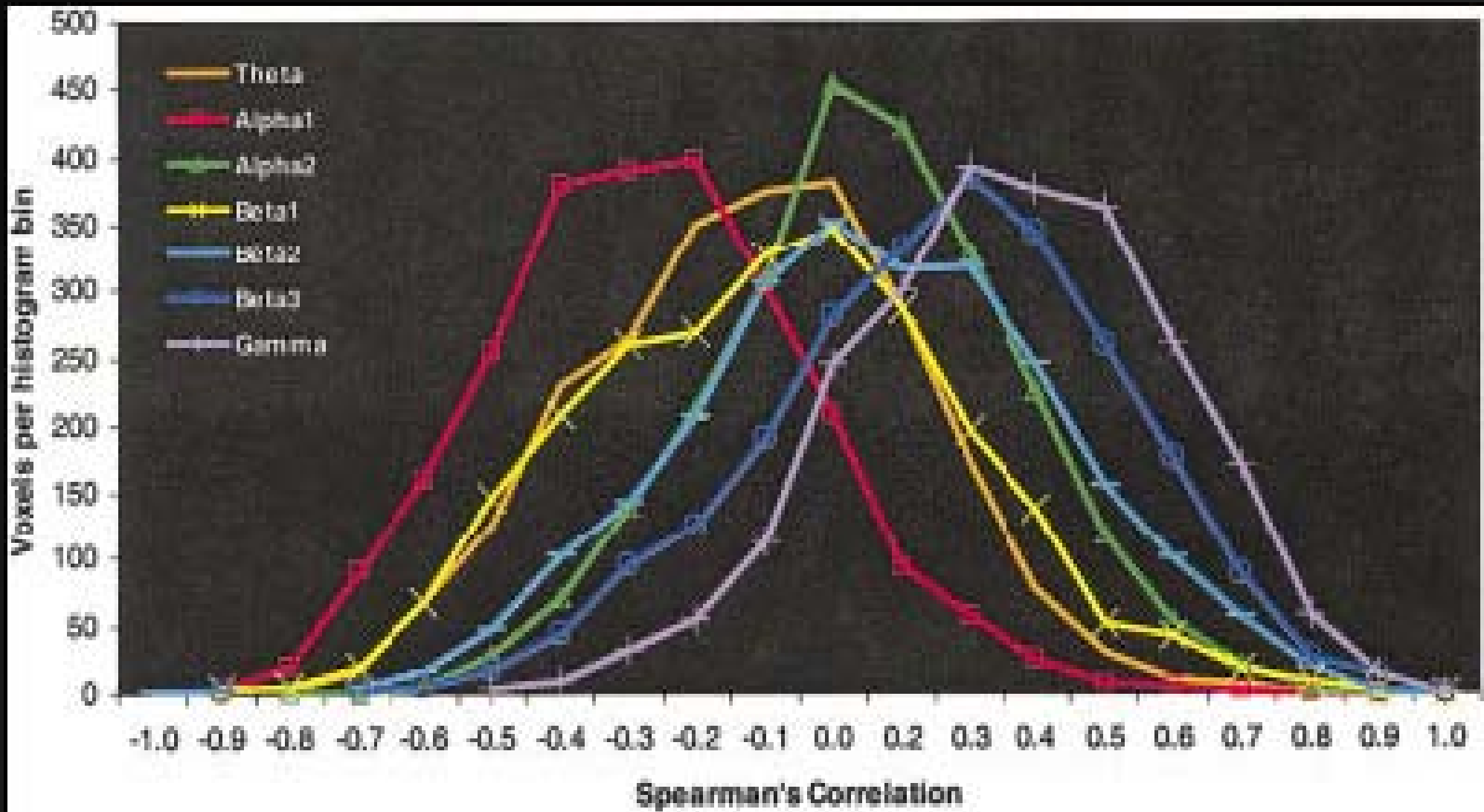
➤ Trait

- Resting EEG asymmetry related to other traits (e.g. BAS)
- Resting EEG asymmetry related to psychopathology (e.g. depression)
- Resting EEG asymmetry predicts subsequent emotional responses (e.g. infant/mom separation)

➤ State

- State EEG asymmetry covaries with current emotional state (e.g., self report, spontaneous emotional expressions)

Alpha Vs Activity Assumption (AAA)



Left Hypofrontality in Depression

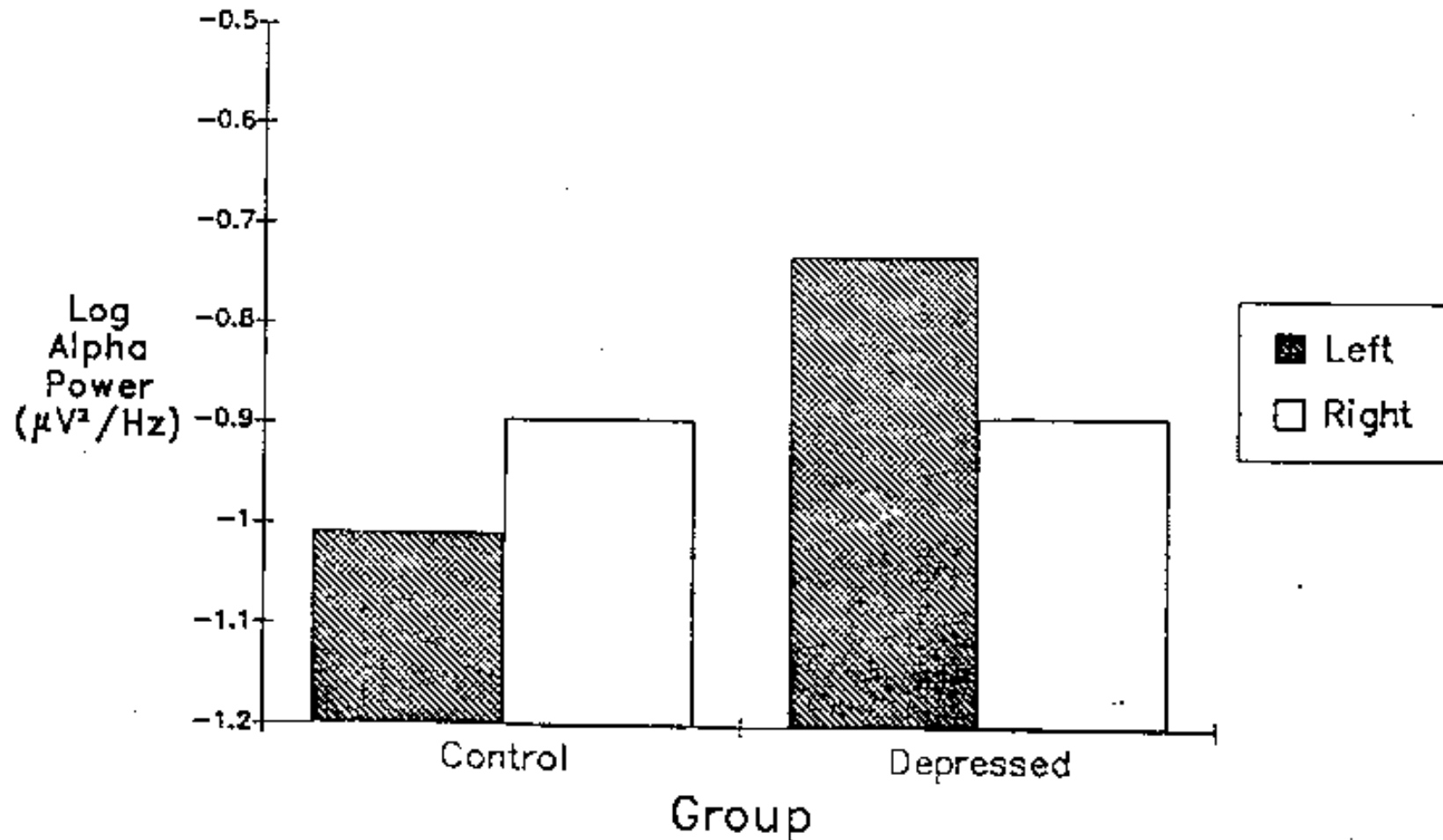
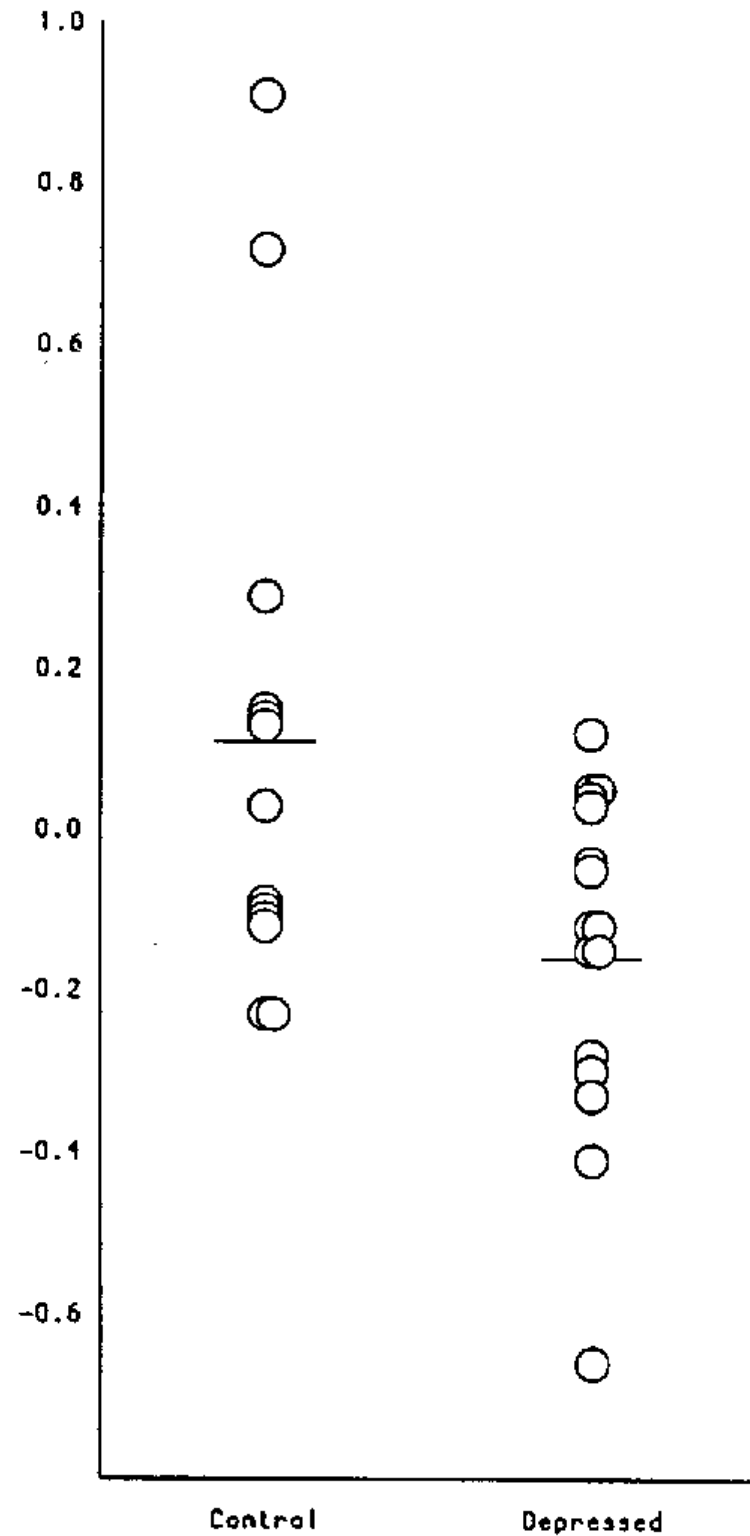


Figure 1. Mean log-transformed alpha (8–13 Hz) power (in $\mu V^2/Hz$) for Cz-referenced electroencephalograms (averaged across eyes-open and eyes-closed baselines), split by group and hemisphere, for the mid-frontal region. (Decreases in alpha power are indicative of increased activation.)

Henriques & Davidson (1991); see also, Allen et al. (1993), Gotlib et al. (1998);
Henriques & Davidson (1990); Reid Duke and Allen (1998); Shaffer et al (1983)

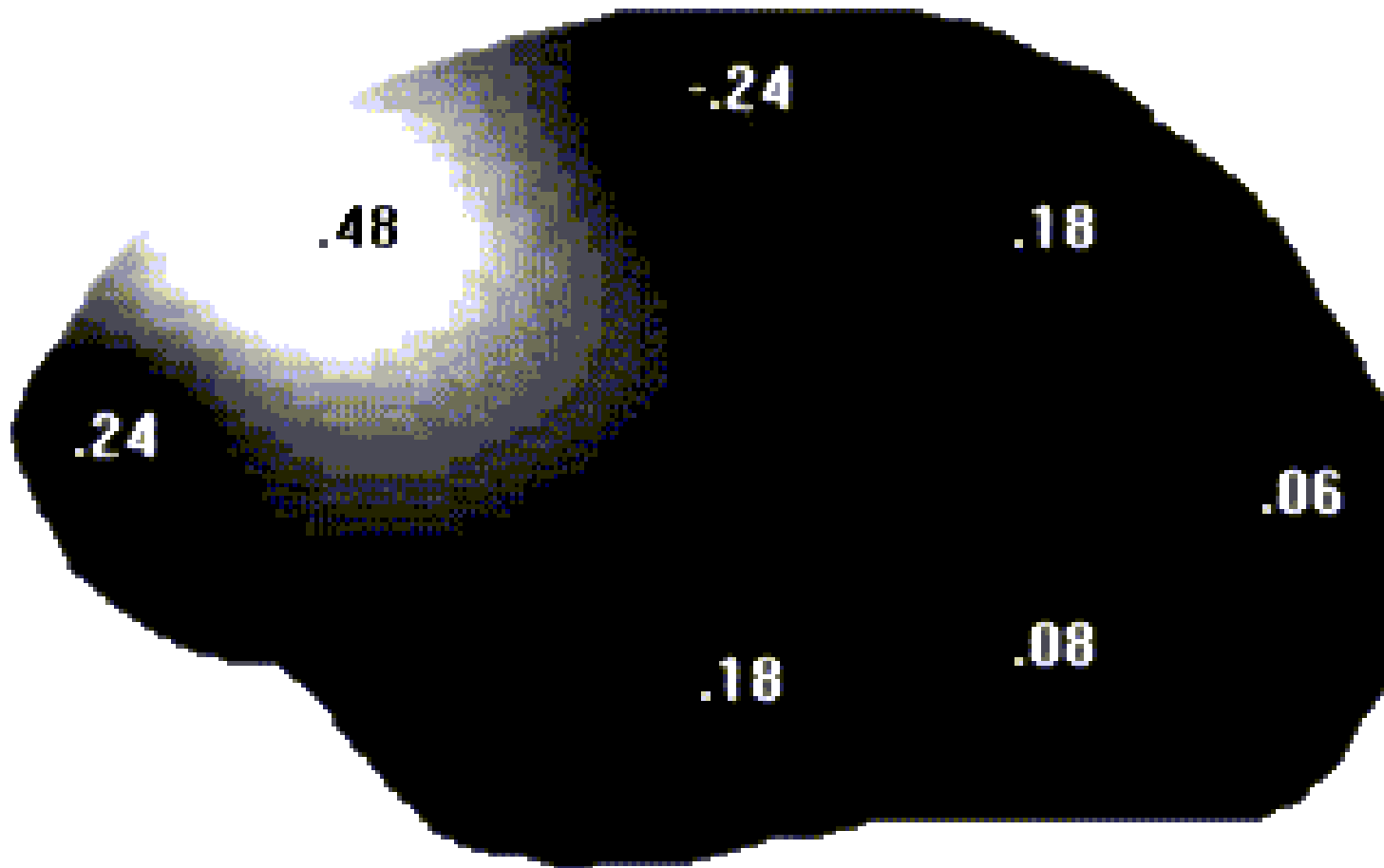
Individual Subjects' Data

Log R-Log L
Alpha Power



Valence Vs Motivation

- Valence hypothesis
 - Left frontal is positive
 - Right frontal is negative
- Motivation hypothesis
 - Left frontal is Approach
 - Right frontal is Withdrawal
- Hypotheses are confounded
 - With possible exception of Anger



Correlation with alpha asymmetry ($\ln[\text{right}] - \ln[\text{left}]$) and trait anger. Positive correlations reflect greater left activity (less left alpha) is related to greater anger. After Harmon-Jones and Allen (1998).

State Anger and Frontal Asymmetry

- Would situationally-induced anger relate to relative left frontal activity?

Method

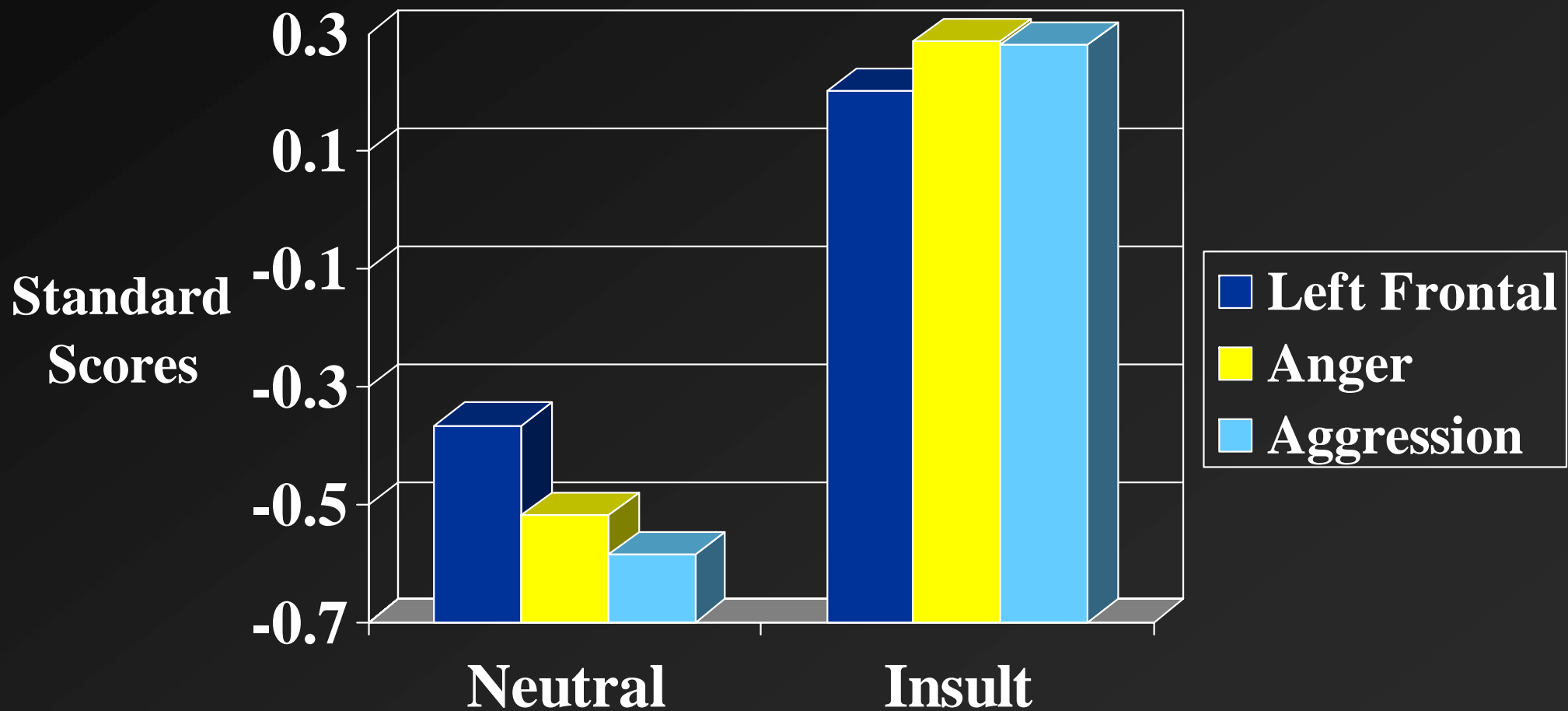
- Cover story: two perception tasks – person perception & taste perception
- Person perception task – participant writes essay on important social issue; another ostensible participant gives written feedback on essay
- Feedback is neutral or insulting
 - negative ratings + “I can’t believe an educated person would think like this. I hope this person learns something while at UW.”

- Record EEG immediately after feedback
- Then, taste perception task, where participant selects beverage for other participant, “so that experimenter can remain blind to type of beverage.”
- 6 beverages; range from pleasant-tasting (sweetened water) to unpleasant-tasting (water with hot sauce)
 - Aggression measure

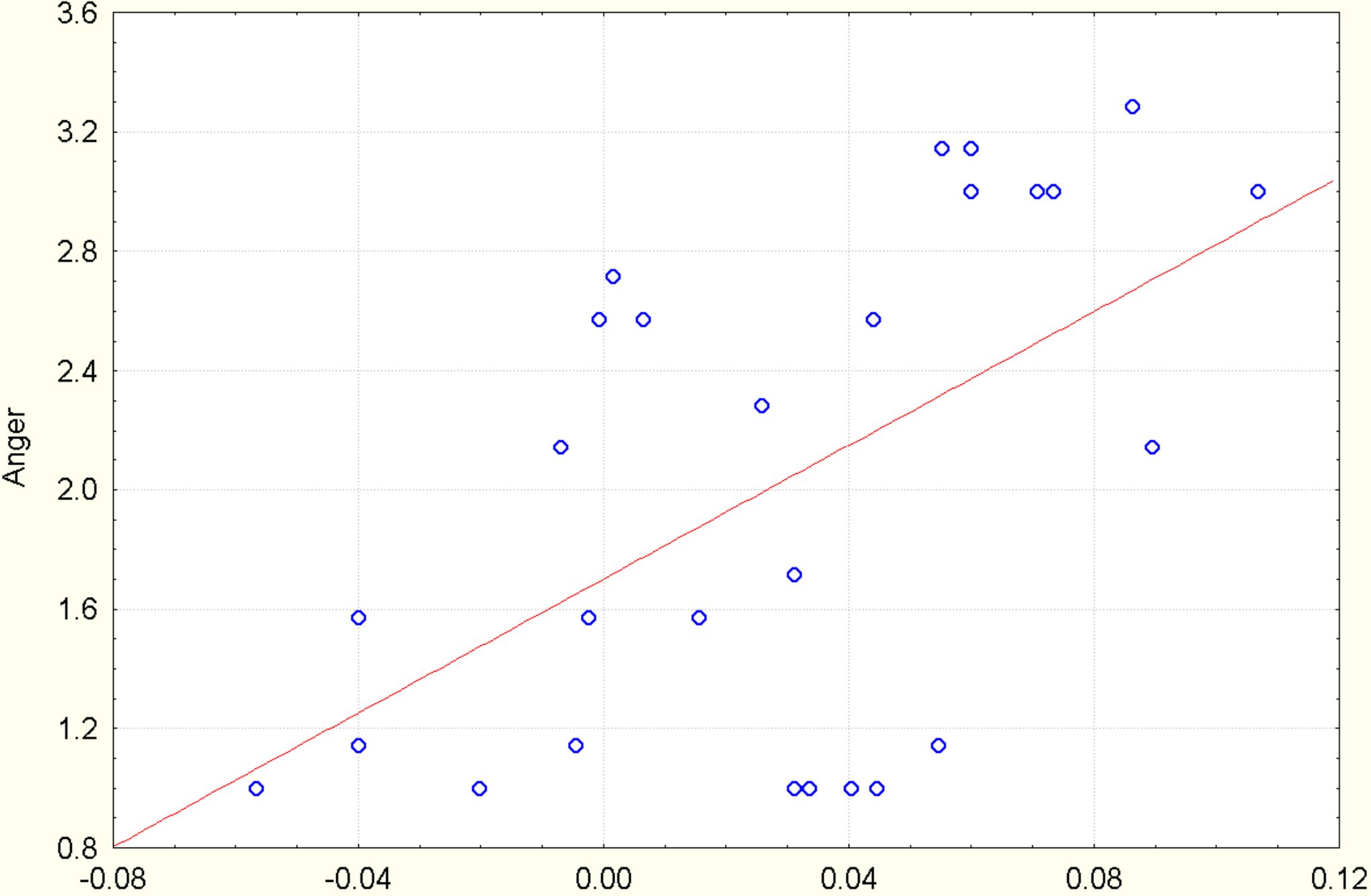


Harmon-Jones & Sigelman, *JPSP*, 2001

Relative Left Frontal, Anger, & Aggression as a Function of Condition



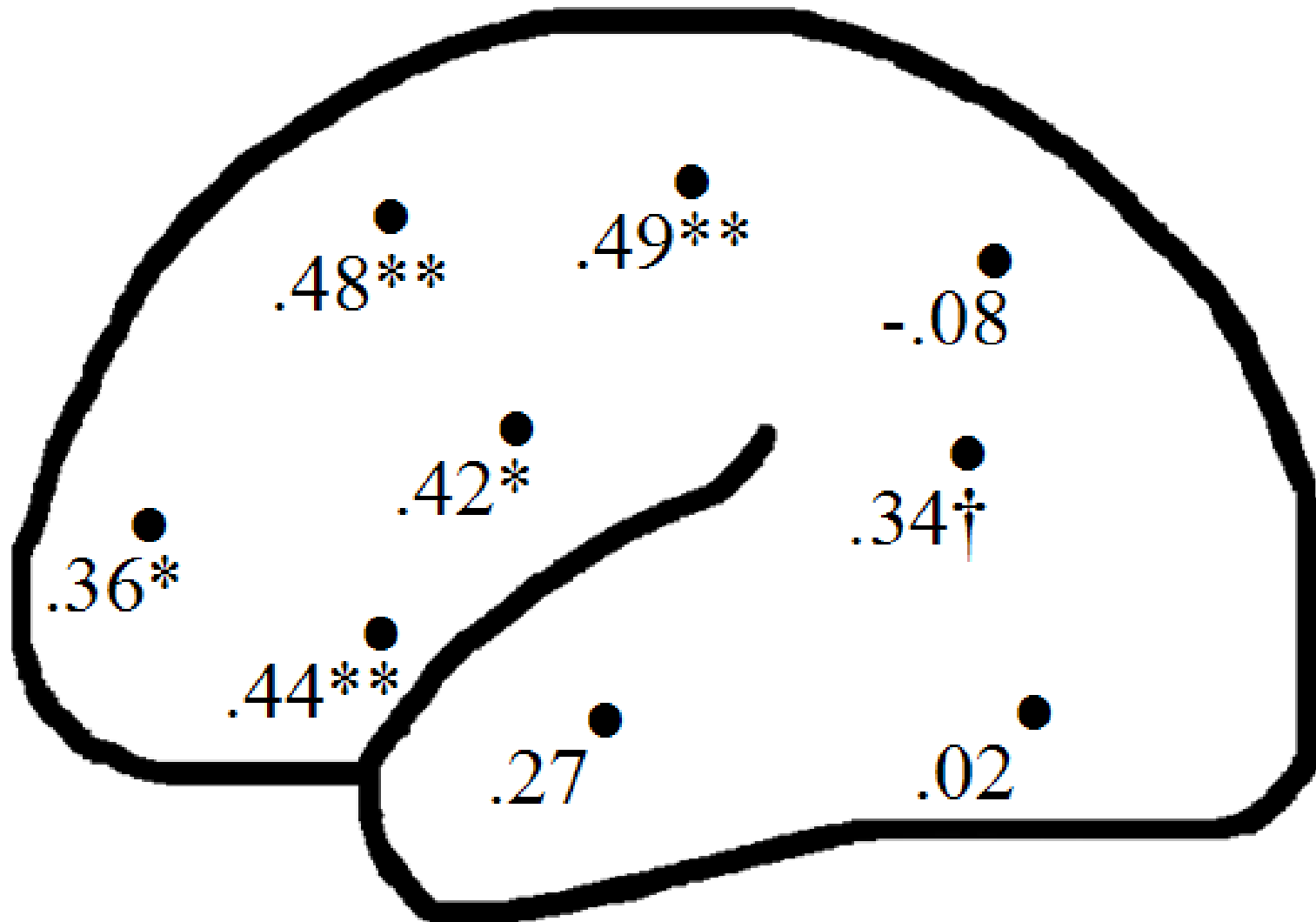
Relationship of State Anger and Relative Left Frontal Activity



Harmon-Jones & Sigelman, *JESP*, 2001

The BAS/BFS/Approach System

- **sensitive to signals of**
 - **conditioned reward**
 - **nonpunishment**
 - **escape from punishment**
- **Results in:**
 - **driven pursuit of appetitive stimuli**
 - **appetitive or incentive motivation**
 - **Decreased propensity for depression (Depue & Iacono, 1989; Fowles 1988)**



Correlations with alpha asymmetry ($\ln[\text{right}] - \ln[\text{left}]$) and self-reported Behavioral Activation Sensitivity. Positive correlations reflect greater left activity (less left alpha) is related to greater BAS scores. From Coan and Allen (2003); see also Harmon-Jones and Allen (1997).

L>R Activity (R>L Alpha) characterizes:

- an approach-related motivational style (e.g. Harmon-Jones & Allen, 1997; Sutton & Davidson, 1997)
- higher positive affect (e.g. Tomarken, Davidson, Wheeler, & Doss, 1992)
- higher trait anger (e.g. Harmon-Jones & Allen, 1998)
- lower shyness and greater sociability (e.g. Schmidt & Fox, 1994; Schmidt, Fox, Schulkin, & Gold, 1999)
- and greater defensiveness (e.g. Kline, Allen, & Schwartz, 1998; Kline, Knapp-Kline, Schwartz, & Russek, in press; Tomarken & Davidson, 1994)

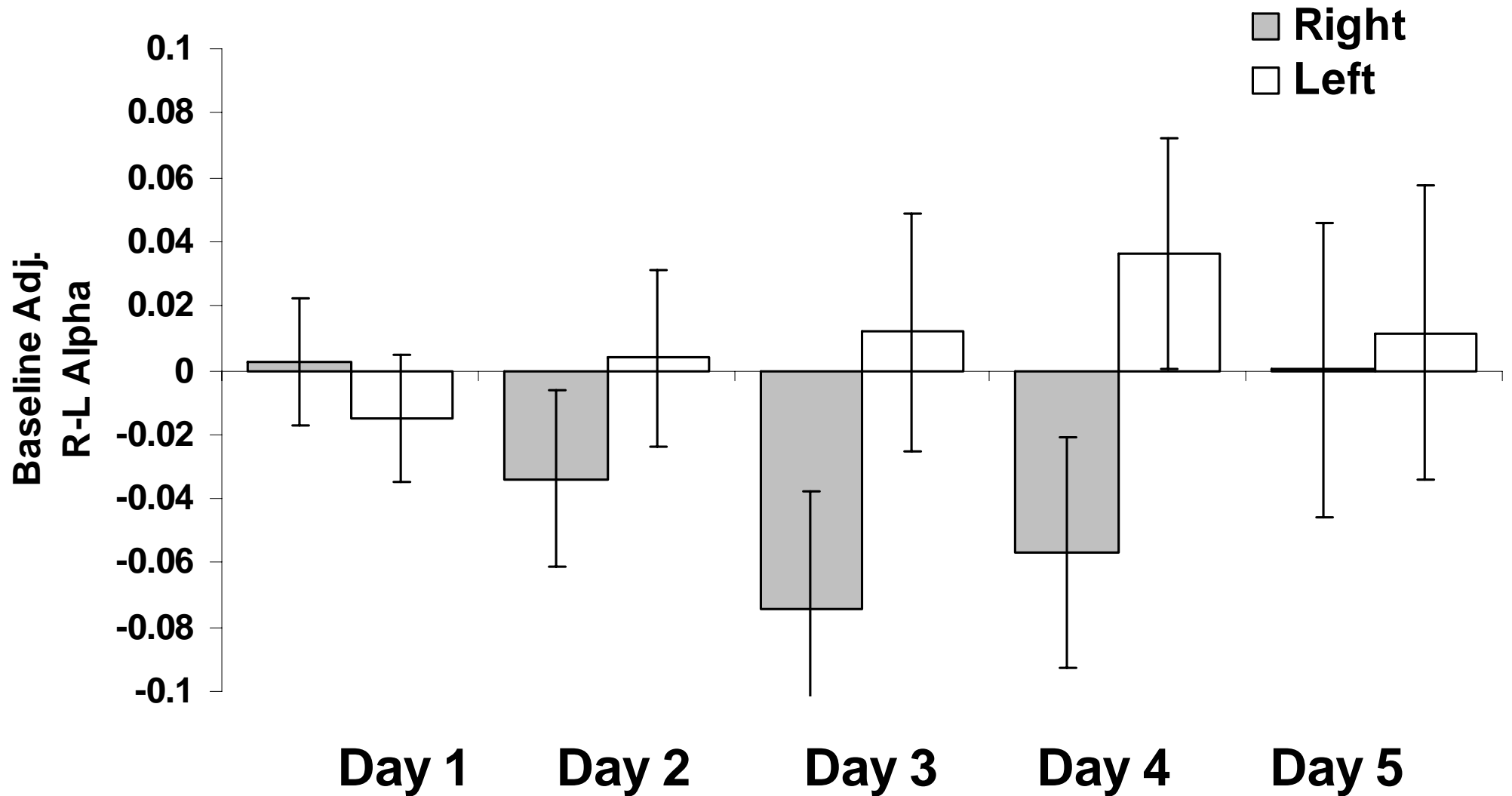
R>L Activity (L>R Alpha) characterizes:

- depressive disorders and risk for depression (e.g. Allen, Iacono, Depue, & Arbisi, 1993; Gotlib, Ranganath, & Rosenfeld, 1998; Henriques & Davidson, 1990; Henriques & Davidson, 1991 **but see also Reid, Duke, & Allen, 1998**)
- certain anxiety disorders (e.g. Davidson, Marshall, Tomarken, & Henriques, 2000; Wiedemann et al., 1999)

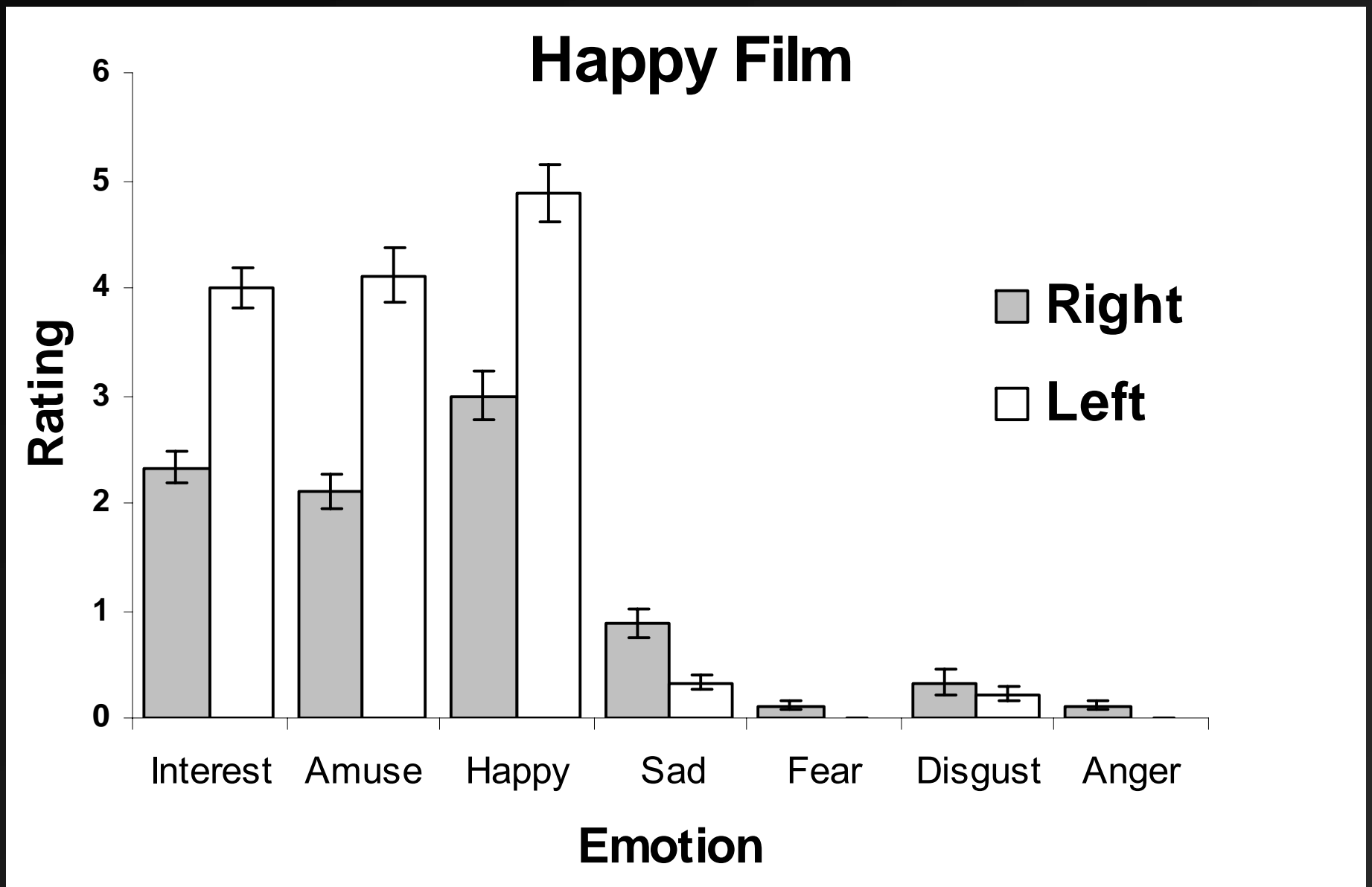
Correlations \neq Causality

- Study to manipulate EEG Asymmetry
- Five consecutive days of biofeedback training (R vs L)
 - Nine subjects trained “Left”; Nine “Right”
 - Criterion titrated to keep reinforcement equal
- Tones presented when asymmetry exceeds a threshold, adjusted for recent performance
- Films before first training and after last training

Training Effects: Asymmetry Scores



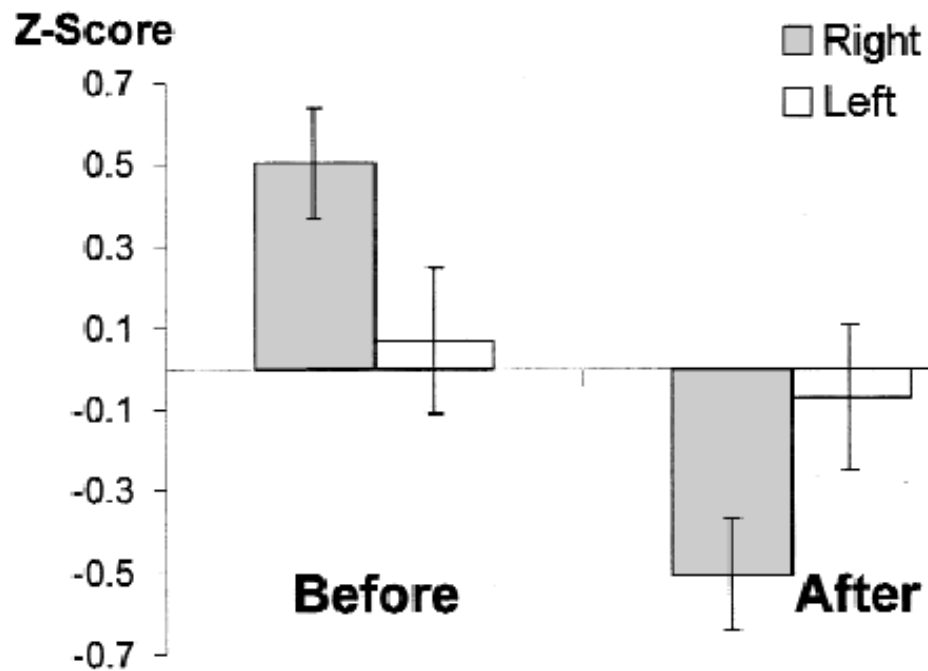
Manipulation of EEG asymmetry with biofeedback produced differential change across 5 days of training; Regression on Day 5



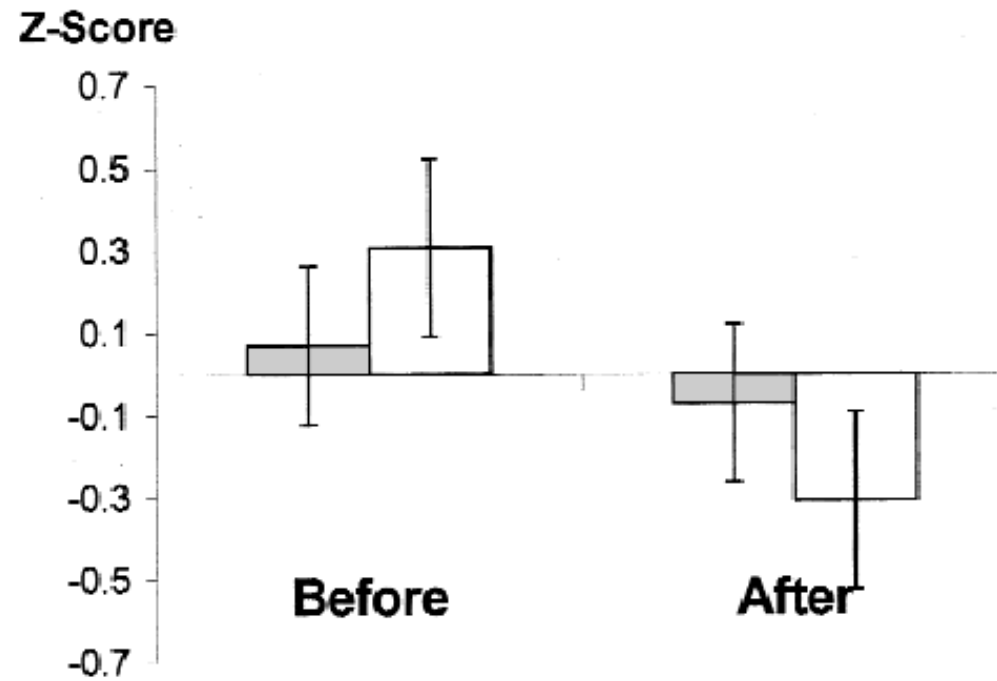
Despite no differences prior to training, following manipulation of EEG asymmetry with biofeedback subjects trained to increase left frontal activity report greater positive affect.

From Allen, Harmon-Jones, and Cavender (2001)

Zygomatic



Corrugator

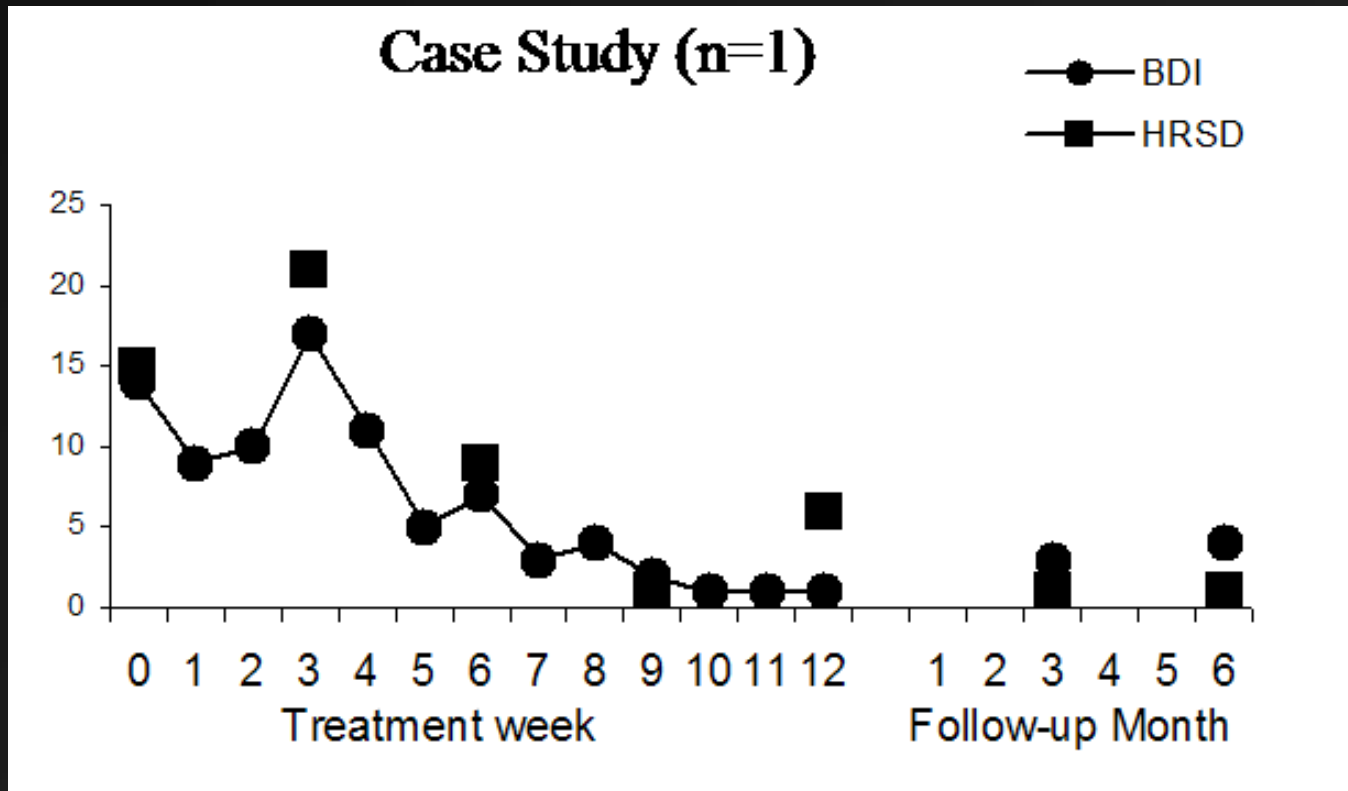


From Allen, Harmon-Jones, and Cavender (2001)

Manipulation of Asymmetry using Biofeedback

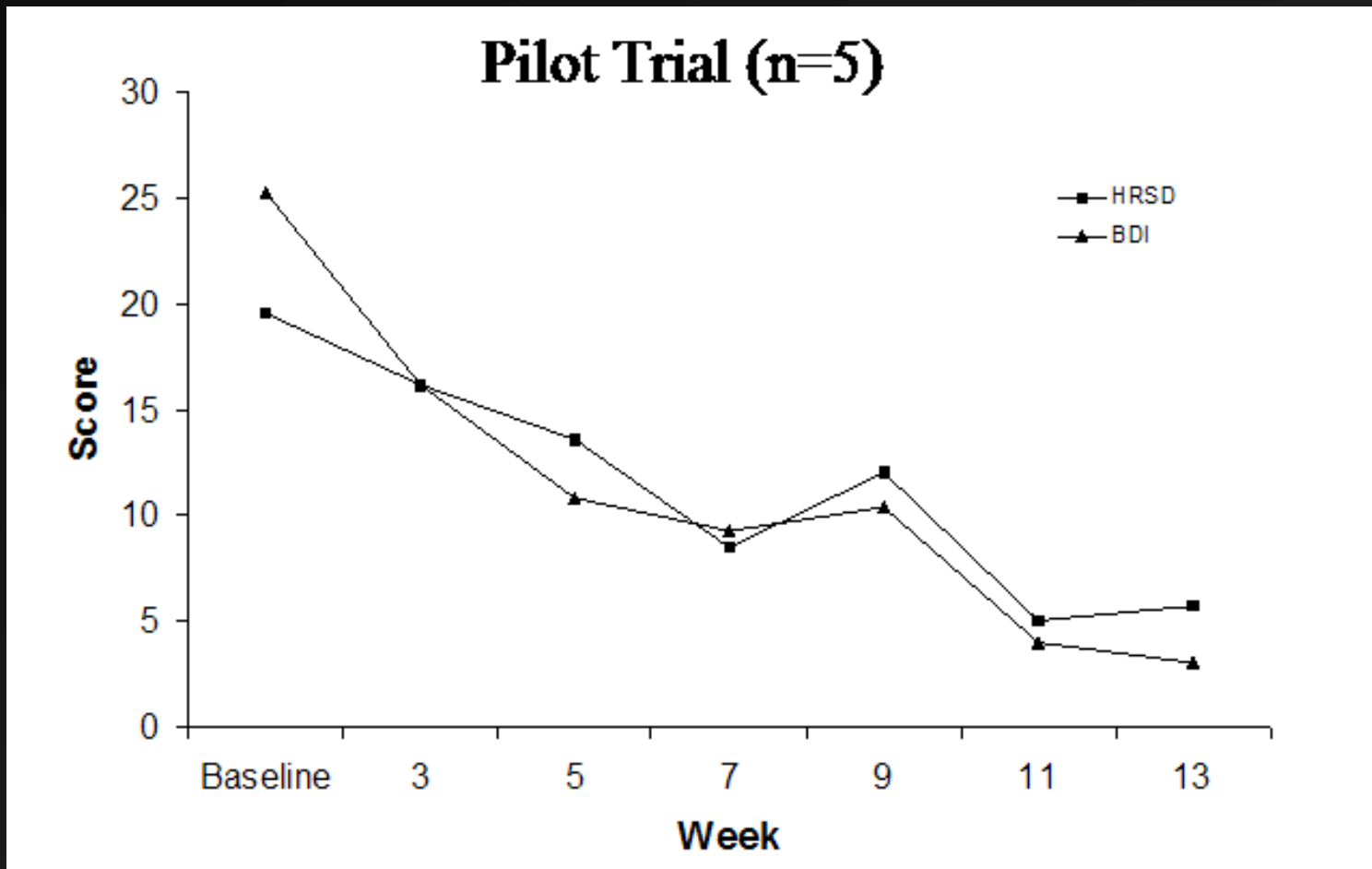
- Phase 1: Demonstrate that manipulation of EEG asymmetry is possible
- Phase 2: Determine whether EEG manipulation has emotion-relevant consequences
- Phase 3: Examine whether EEG manipulation produces clinically meaningful effects
- Phase 4: Conduct efficacy trial

Phase 3a



Biofeedback provided 3 times per week for 12 weeks

Phase 3b



“Open Label” pilot trial, with biofeedback provided 3 times per week for 12 weeks

Phase 4: Randomized Control Trial

- Depressed subjects ages 18-60 to be recruited through newspaper ads
- Ad offers treatment for depression but does not mention biofeedback
- Participants meet DSM-IV criteria for Major Depressive Episode (nonchronic)

Design

- Contingent-noncontingent yoked partial crossover design
- Participants randomly assigned to:
 - *Contingent Biofeedback*: tones presented in response to subject's EEG alpha asymmetry
 - *Noncontingent Yoked*: tones presented that another subject had heard, but tones not contingent upon subject's EEG alpha asymmetry
- Treatments 3 times per week for 6 weeks
- After 6 weeks, all subjects receive contingent biofeedback 3 times per week for another 6 weeks

Results

A Different Manipulation

Peterson, Shackman, Harmon-Jones (2008)

- Hand contractions to activate contralateral premotor cortex
- Insult about essay (similar to Harmon-Jones & Sigelman, *JPSP*, 2001) followed by chance to give aversive noise blasts to the person who insulted them
- Hand contractions:
 - altered frontal asymmetry as predicted
 - Altered subsequent aggression (noise blasts)
- Asymmetry during hand contractions predicted aggression

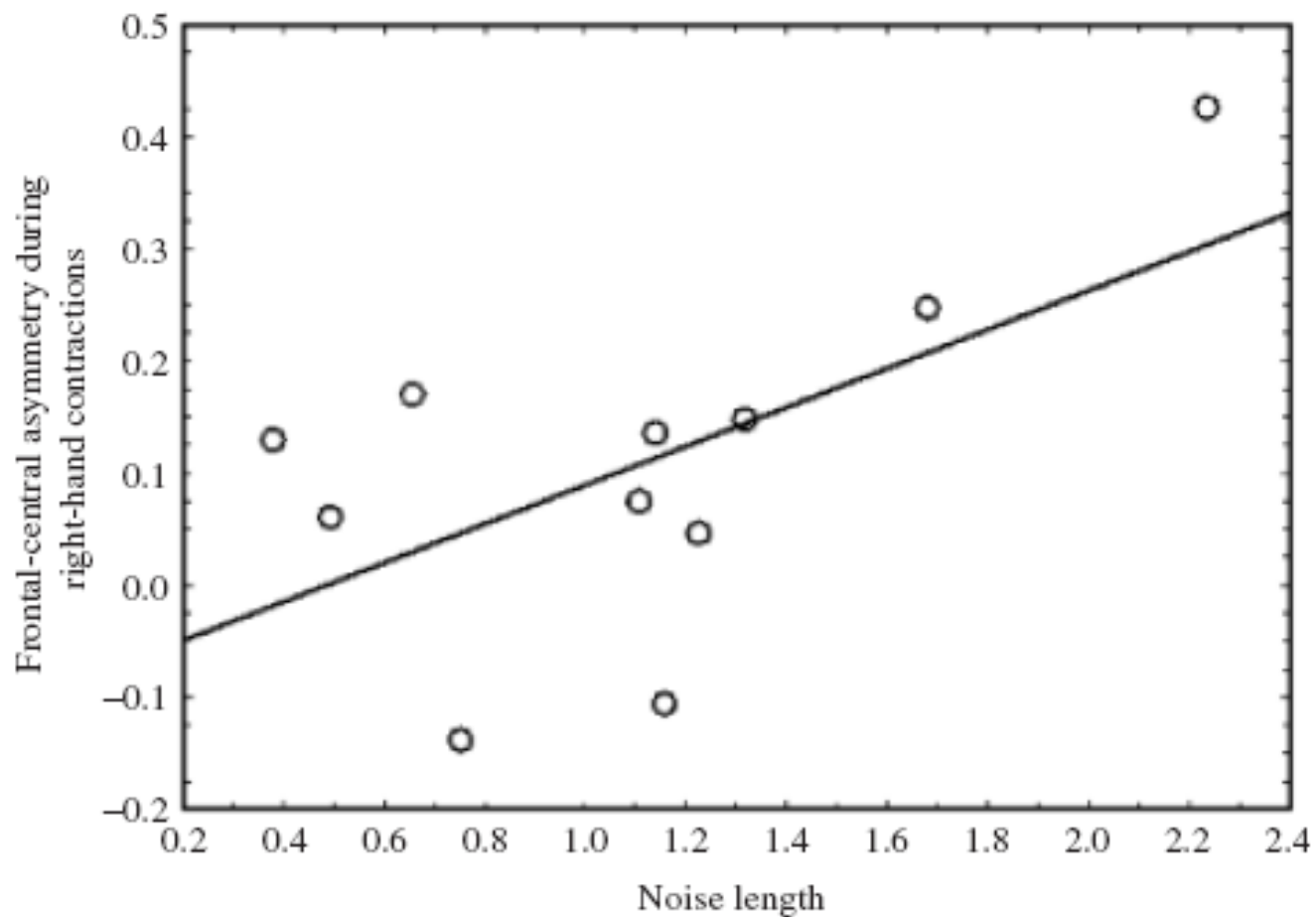


Figure 1. Relation between noise length and frontal-central asymmetry during right-hand contractions. Higher asymmetry scores indicate greater relative left than right activation.

State Changes

➤ Infants

- Stanger/Mother paradigm (Fox & Davidson, 1986)
- Sucrose Vs water (Fox & Davidson, 1988)
- Films of facial expressions (Jones & Fox, 1992; Davidson & Fox, 1982)

➤ Primates

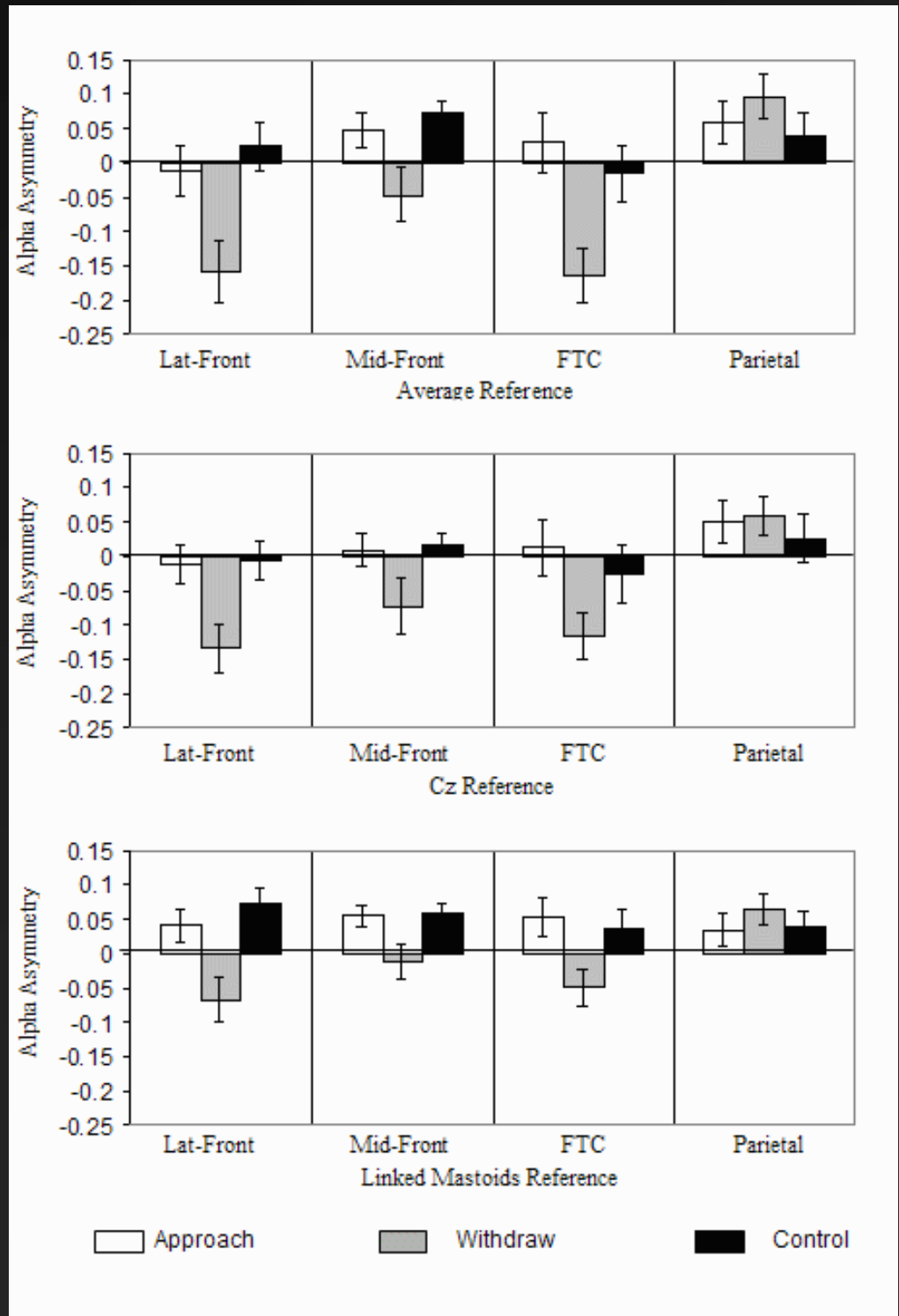
- Benzodiazepines increases LF (Davidson et al., 1992)

State Changes

- Adults
 - Spontaneous facial expressions (Ekman & Davidson, 1993; Ekman et al., 1990; Davidson et al., 1990)
 - Directed facial actions (Coan, Allen, & Harmon-Jones, 2001)

EEG responds to directed facial actions

From Coan, Allen, and Harmon-Jones (2001)



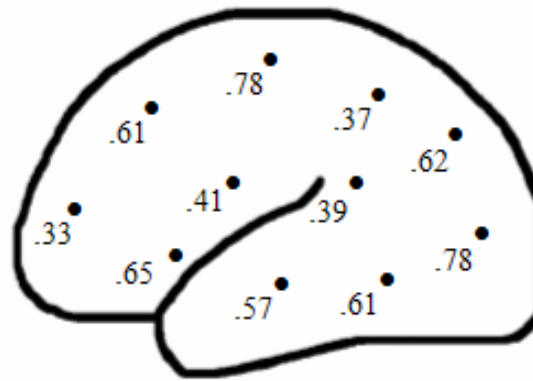
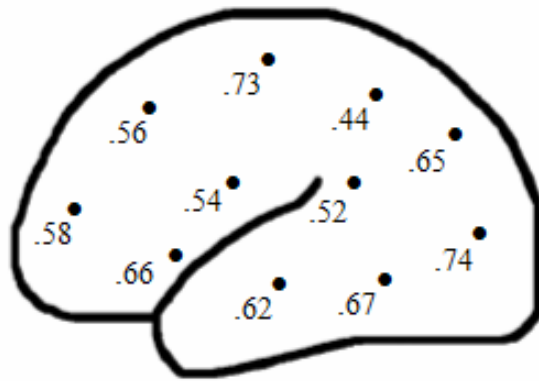
Can EEG Asymmetry serve as Trait Indicator of Risk for _____?

- test-retest stability in nonclinical populations
 - ICCs .53 to .72 across three weeks (Tomarken et al., 1992)
 - ICC of .57 for five sessions across two years (Tomarken et al., 1994)
 - Correlation of .66 between asymmetry at 3 months and asymmetry at 3 years of age (Jones et al., 1997)
 - 52-64% of variance across 4 sessions due to temporally stable latent trait (Hagemann et al., 2002)
- Test-retest stability in depressed folks (Allen et al., 2004)
 - median ICC across three assessments was .56, .76, .41 for AR, Cz, and LM referenced data
 - across five assessments, the comparable medians were .61, .60, and .61 for AR, Cz, and LM referenced data.

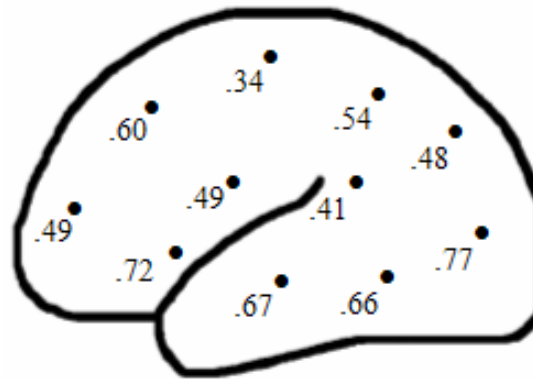
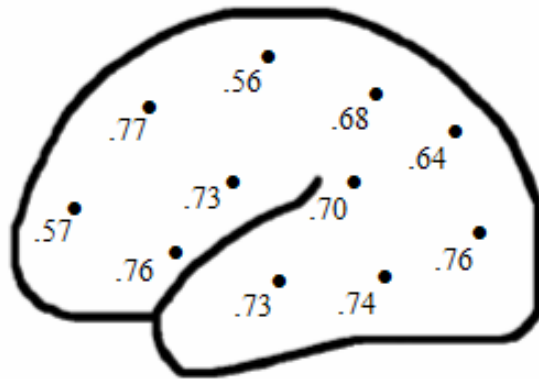
Three Assessments

Five Assessments

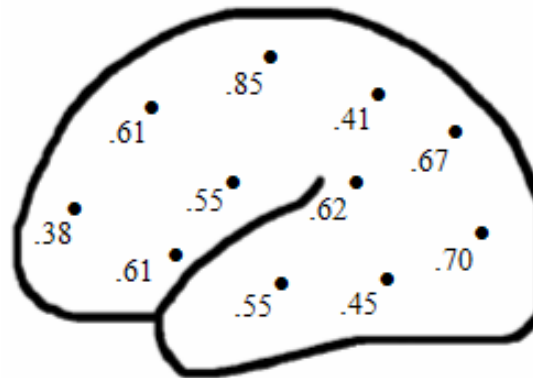
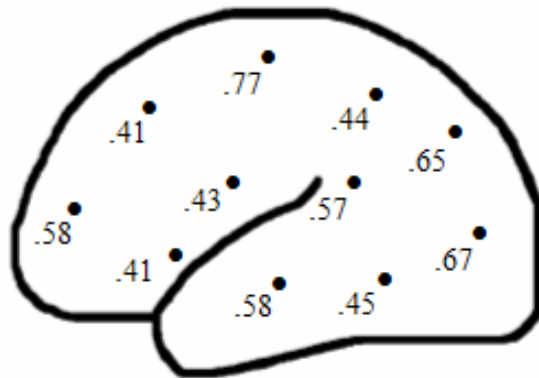
**Average
Reference**



**Cz
Reference**



**“Linked”
Mastoids
Reference**



Allen, Urry, Hitt,
& Coan (2004),
Psychophysiology

| Episode | Liability | Genetic |
|--|--|--|
| Characterizes most depressed persons (sensitivity) ^{1,4,5,8,-9,11} | Characterizes most depressed persons (sensitivity) ^{1,4,5,8,-9,11} | Characterizes most depressed persons (sensitivity) ^{1,4,5,8,-9,11} |
| Differentiates depressed from nondepressed (specificity) ^{1,-3,4,5-6,-13} | Differentiates depressed from nondepressed, not only in episode but in remission as well ^{1,-3,7} | Differentiates depressed from nondepressed, not only in episode but in remission as well ^{1,-3,7} |
| Changes with variations in clinical state ¹⁰ | Demonstrates stability in both depressed and nondepressed individuals ^{1,-4,12,present report} | Demonstrates stability in both depressed and nondepressed individuals ^{1,-4,12,present report} |
| | Predicts the future development of depression in individuals currently not depressed ^{NA} | Predicts the future development of depression in individuals currently not depressed ^{NA} |
| | | Is heritable within the normal population ² |
| | | Is more common in depressed persons with a strong family history of depression than those without a such a history ^{NA} |
| | | Is more prevalent in families of depressed individuals than in families of nondepressed individuals ^{NA} |
| | | Identifies those family members at risk for depression ^{NA} |

¹Allen et al., 1993

²Allen, Reiner, Katsanis, & Iacono, 1997

³Davidson et al., 2000

⁴Debener et al., 2000

⁵Gotlib et al., 1998

⁶Heller et al., 1997

⁷Henriques & Davidson, 1990

⁸Henriques & Davidson, 1991

⁹Reid et al., 1998

¹⁰Rosenfeld, Baehr, Baehr, Gotlib, & Ranganath, 1996

¹¹Schaffer et al., 1983

¹²Tomarken, Davidson, Wheeler, & Kinney, 1992

¹³Wiedemann et al., 1999

Heritability of EEG Power Spectra

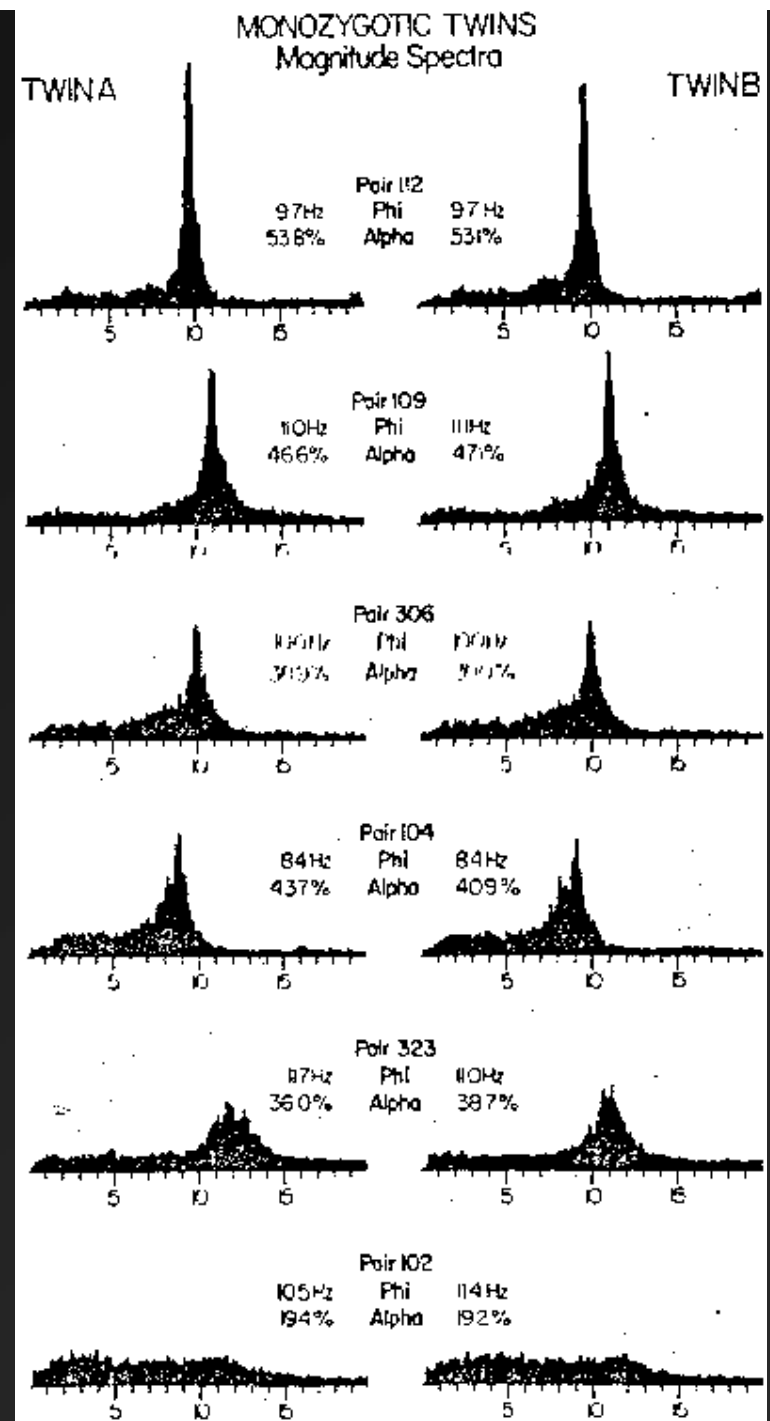


Figure 1. EEG spectra from 6 of the 39 monozygotic (MZ) twin pairs studied in 1974, selected to show the range of amount of alpha activity. Phi is the median frequency in a 3-Hz band centered on the central peak. All spectra are standardized to unit area. (Reprinted from Lykken, Tellegen, & Thorkeison, 1974.)

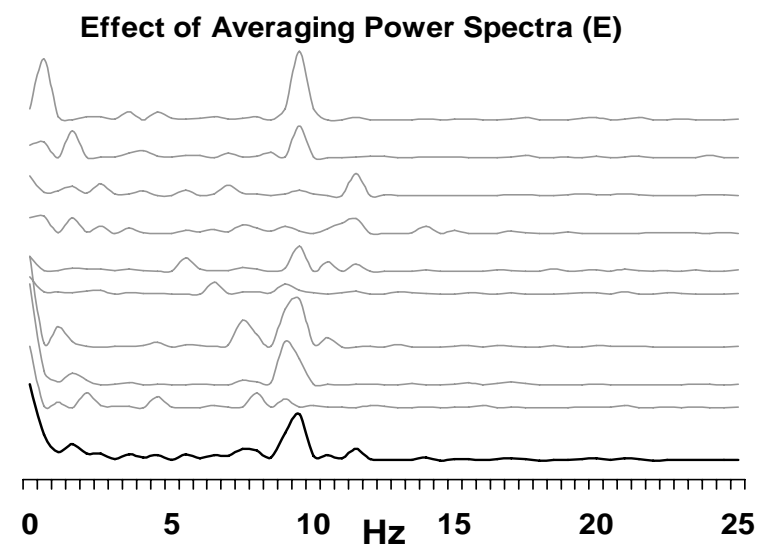
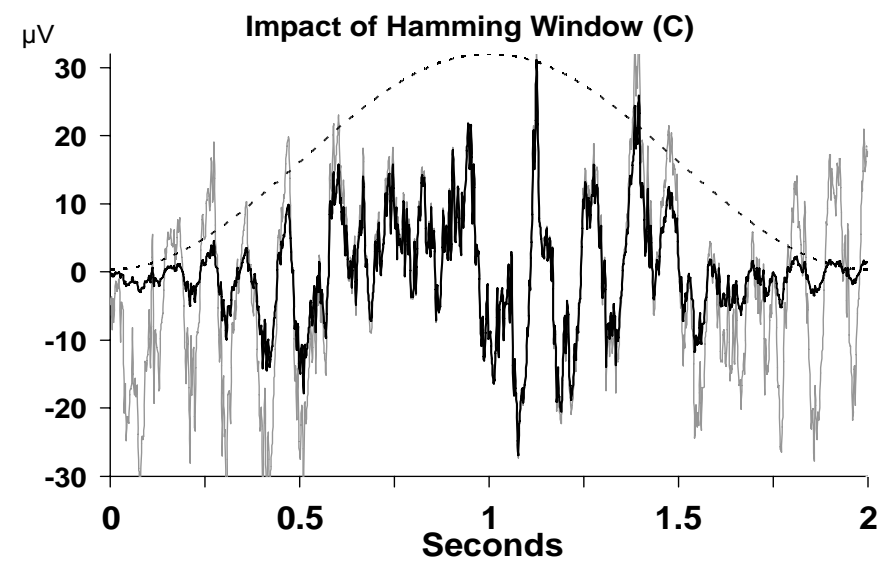
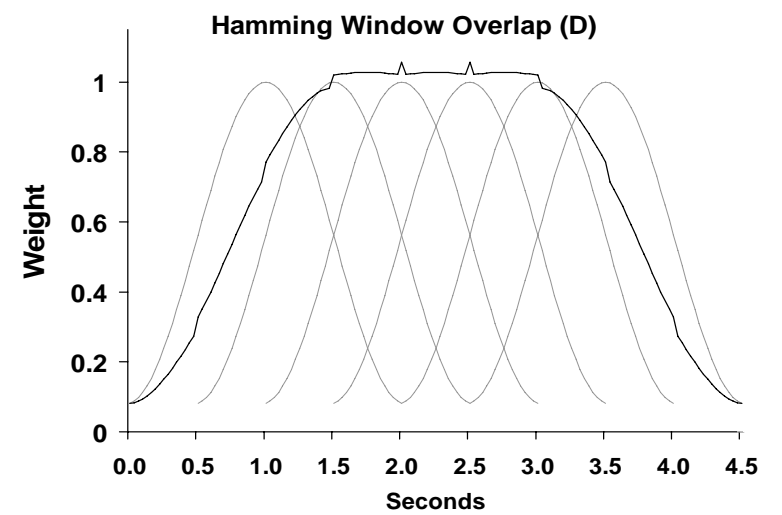
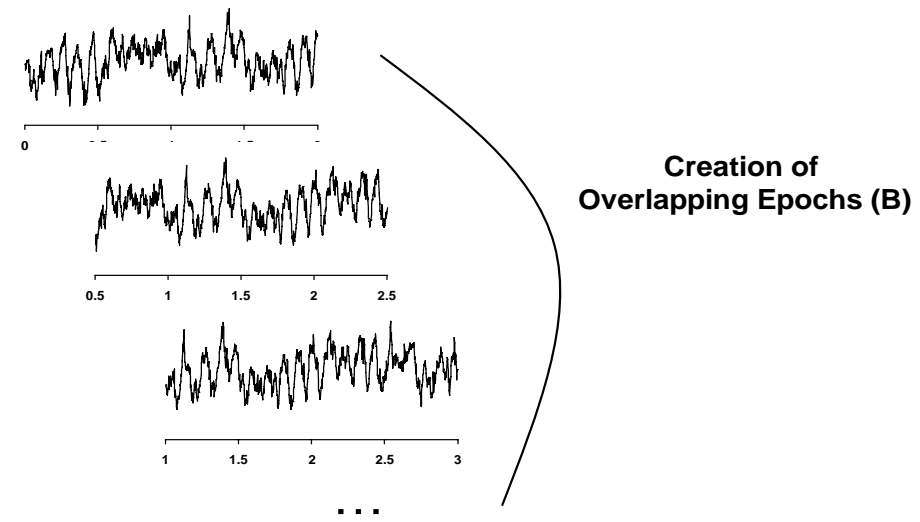
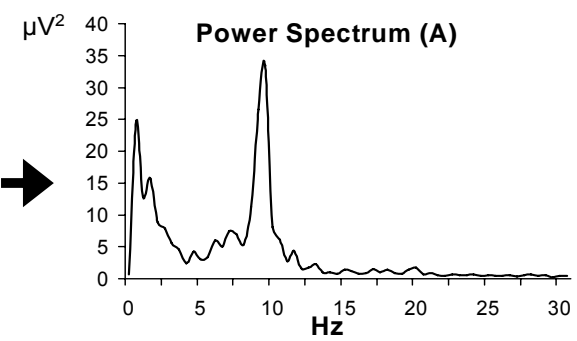
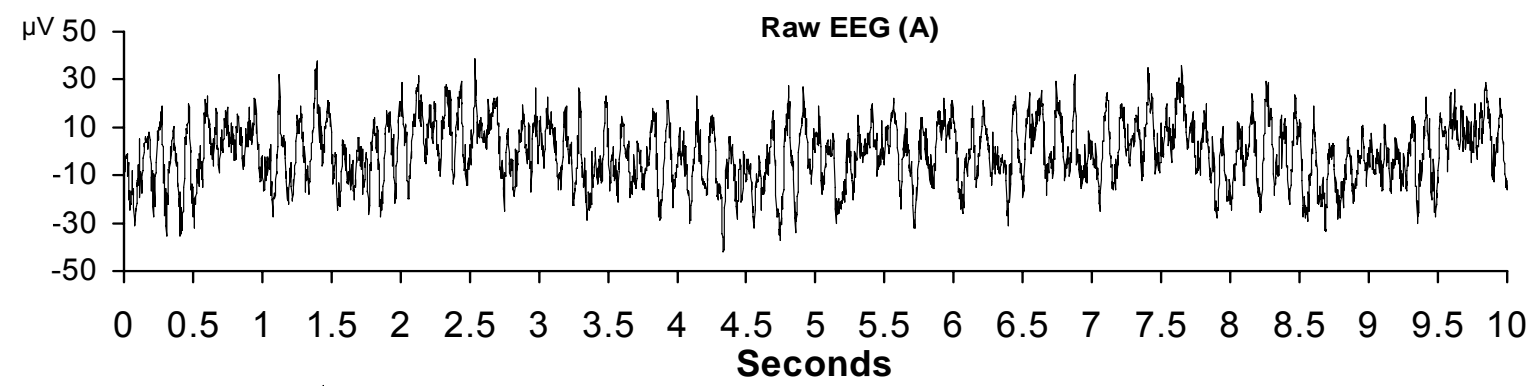
Trait, Occasion, and State variance

- Three sources of reliable variance for EEG Asymmetry
 - *Stable trait consistency* across multiple assessments
 - *Occasion-specific* variance
 - reliable variations in frontal asymmetry across multiple sessions of measurement
 - may reflect systematic but unmeasured sources such as current mood, recent life events and/or factors in the testing situation.
 - *State-specific* variance
 - changes within a single assessment that characterize
 - the difference between two experimental conditions
 - the difference between baseline resting levels and an experimental condition.
 - conceptualized as proximal effects in response to specific experimental manipulations
 - should be reversible and of relatively short duration
- Unreliability of Measurement (small)

Synopsis of Signal Processing and...

Issues and Assumptions on the Road from Raw Signals to Metrics of Frontal EEG Asymmetry in Emotion

These next few slides and concepts based loosely on the best-selling manuscript of the same name by Allen, Coan, & Nazarian (2004)

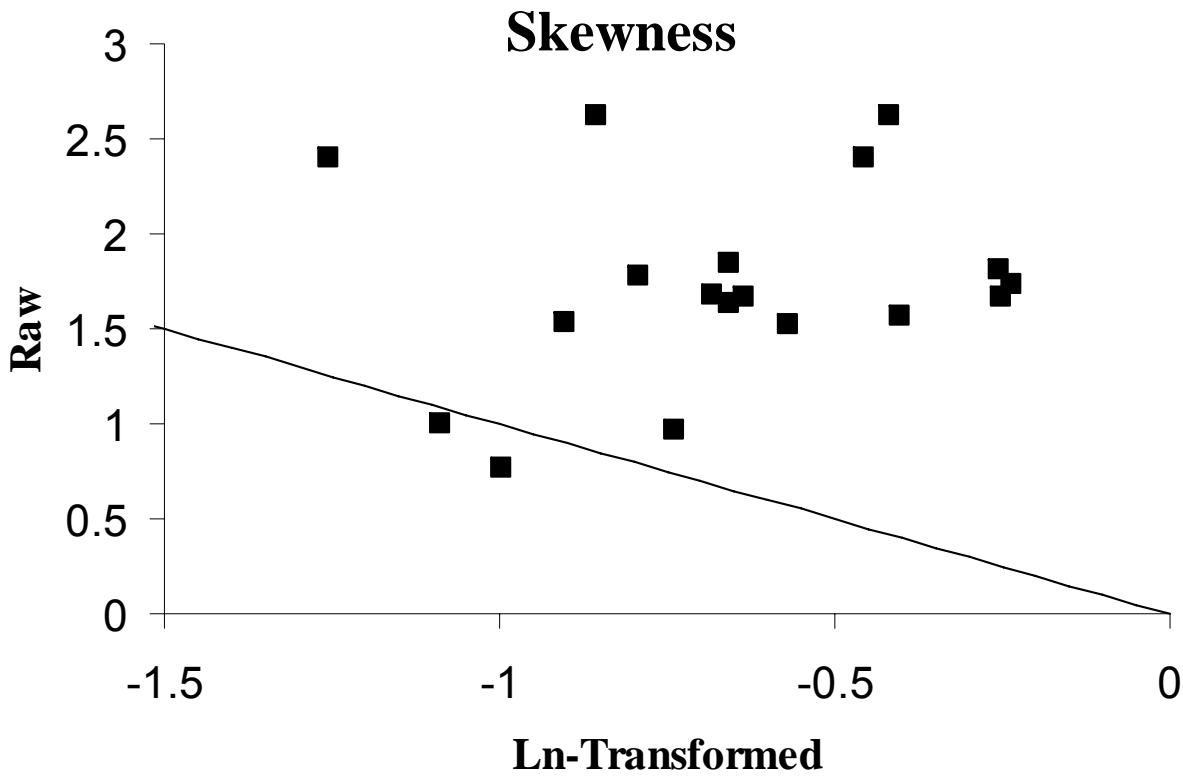


Assessing Asymmetry

- Difference Score
 - Sites typically natural log transformed prior to taking difference
 - Right minus left alpha: $\ln(Right) - \ln(Left)$
- Higher Scores:
 - Greater relative right alpha
 - By inference, less relative right activity

(Natural) Log Transforms

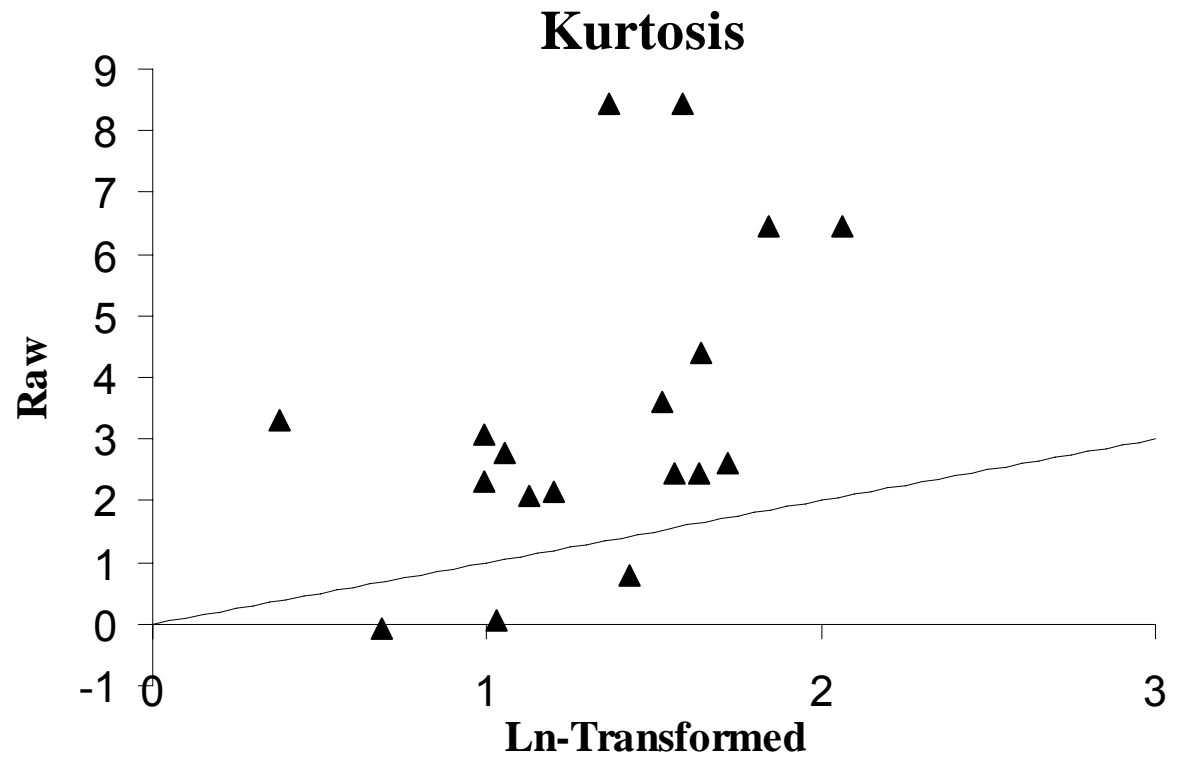
- Why?
 - Everyone is doing it!
 - Folks say power values are skewed



Transformation improves skewness for 89% of the scalp sites, and improves kurtosis for 83% of the scalp sites

% Sites deviating from Normality

| | Before Ln- Transform | After Ln- Transform |
|----------|----------------------------|---------------------------|
| Skewness | 94% | 33% |
| Kurtosis | 83% | 39% |



Difference of ln-Transforms

- Individual sites are therefore ln-transformed prior to taking the difference score

% Asymmetry scores deviating from Normality

| | Before Ln- Transform | After Ln- Transform |
|----------|----------------------------|---------------------------|
| Skewness | 67% | 22% |
| Kurtosis | 67% | 33% |

Asymmetry Metric Vs Individual Sites

- Is it left or is it right?
- Can assess using ANOVA with hemisphere as a factor
 - Removes overall power before testing for interaction of emotion/temperament/psychopathology with hemisphere
 - But not easily amenable for assessing relationship of EEG at given site to continuous variables

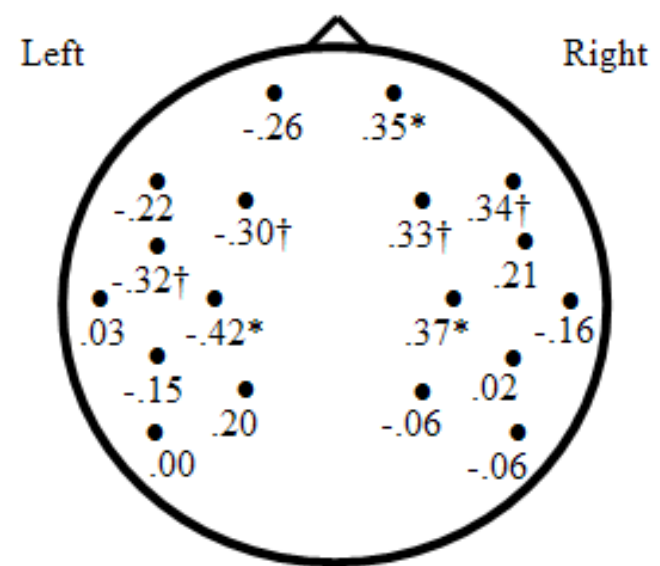
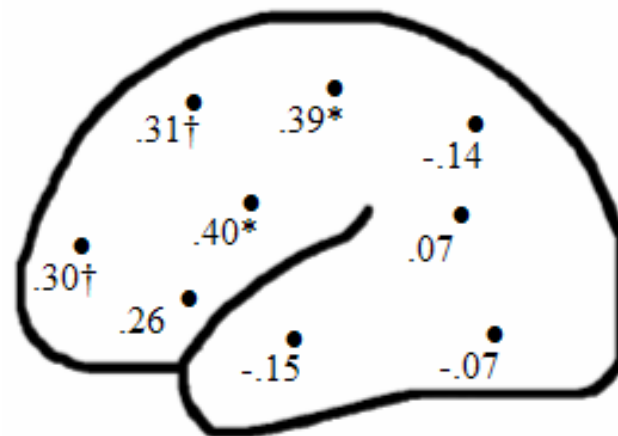
Asymmetry Metric Vs Individual Sites

- The Problem:
 - Power at an individual site reflects:
 - Underlying neural activity
 - Scalp thickness
- An early (nonoptimal) solution
 - Residualize power at each lead based on
 - Whole head power (reasonable)
 - Homologous lead power (troublesome)

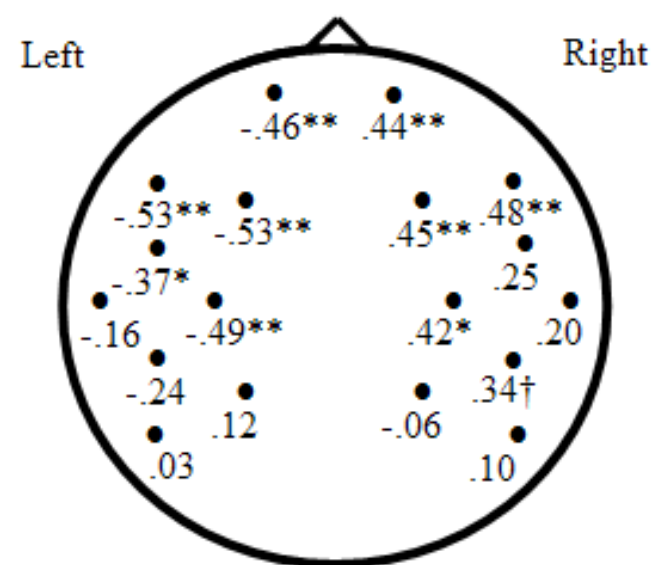
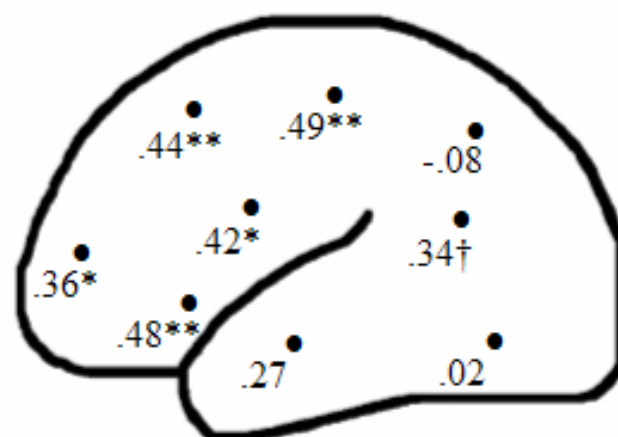
Ln(Right)-Ln(Left)

Residualized Power

Average Reference



Linked Mastoids Reference



†p < .10; *p < .05; ** p < .01

Why does it do *that*?!

- This double residualization results in correlations with the outcome variable similar in magnitude to the difference score, but with opposite signs for the two hemispheres.
- This is actually to be expected when the predictor and criterion variable are highly correlated

Alpha Power at Homologous Sites is *Highly* Correlated

| Sites | Reference | |
|--------------|-----------|------|
| | AR | LM |
| FP1 .. FP2 | .997 | .998 |
| F7 .. F8 | .983 | .971 |
| F3 .. F4 | .990 | .992 |
| FTC1 .. FTC2 | .975 | .943 |
| C3 .. C4 | .977 | .981 |
| T3 .. T4 | .918 | .891 |
| TCP1 .. TCP2 | .944 | .948 |
| P3 .. P4 | .965 | .982 |
| T5 .. T6 | .907 | .932 |

Consider residualized left lead power when $L \approx R$

$$L_{resid} = L - \hat{L}$$

$$\hat{L} = a + b(R)$$

In limiting case where $r_{lr} \rightarrow 1.0$

$$\hat{L} = 0 + 1(R) = R$$

$$L_{resid} = L - \hat{L} = L - R$$

Fancy That!

- Residual values for left hemisphere leads approaches $L - R$ as the correlation between left and right leads approaches 1.0.
- Residual values for right hemisphere approaches the value $R - L$ as the correlation between left and right leads approaches 1.0.
- Therefore, this procedure will make it appear that right hemisphere leads correlate with a criterion variable in the same direction and magnitude as the $R - L$ difference score, and that left hemisphere leads correlate with a criterion variable in the opposite direction but same magnitude as the $R - L$ difference score.
- Therefore, *don't do that!*